

Laboratorio de Sistemas Dinámicos



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SCHOOL ON NONLINEAR DYNAMICS, COMPLEX NETWORKS, INFORMATION THEORY AND MACHINE LEARNING IN NEUROSCIENCE ICTP-SAIFR - São Paulo, Brasil – May 22 - 26, 2023







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Interdisciplinary work in neuroscience

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The goal of our research is to shed light on the dynamical mechanisms involved in the perception and the generation of complex sounds and to study the brain and the peripheral system in this process. **Dynamical** Systems models **Behavior**: Laboratori Neural recording Sistemas recordings **Minamico** and analysis Muscle & respiratory recordings





Lecture 1

Introduction to nonlinear dynamics and excitable systems

Lecture 2

Dynamical models for single neurons. Comparison with experimental data.

Lecture 3

The neuroethology perspective in neuroscience. Case of study: models of vocal production in birds.







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Lecture 1 Introduction to nonlinear dynamics and excitable systems Ana Amador

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Definition : set of **variables** that describe state of the system and a **law** that describes the evolution of the state variables with time

how the state of the system in the next moment of time depends on the input and its state in the previous moment of time

Example:

The Hodgkin-Huxley model

(4-dimensional dynamical system) Its state is uniquely determined by the membrane potential, V , and the "gating variables" n, m, and h for persistent K+ and transient Na+ currents.

The evolution law is given by a **4-dimensional system of ordinary differential equations.**

$$C\dot{V} = I - \overbrace{\overline{g}_{\mathrm{K}}n^{4}(V - E_{\mathrm{K}})}^{I_{\mathrm{K}}} - \overbrace{\overline{g}_{\mathrm{Na}}m^{3}h(V - E_{\mathrm{Na}})}^{I_{\mathrm{Na}}} - \overbrace{\overline{g}_{\mathrm{L}}(V - E_{\mathrm{L}})}^{I_{\mathrm{L}}}$$

$$\dot{n} = \alpha_{n}(V)(1 - n) - \beta_{n}(V)n$$

$$\dot{m} = \alpha_{m}(V)(1 - m) - \beta_{m}(V)m$$

$$\dot{h} = \alpha_{h}(V)(1 - h) - \beta_{h}(V)h ,$$

Is this dynamical system nonlinear?



Nonlinear Dynamics

Nonlinear rules

Mechanisms responsible for governing the temporal evolution of a system

Let's see...

$$C\dot{V} = I - \overbrace{\overline{g_{\mathrm{K}}n^{4}}(V - E_{\mathrm{K}})}^{I_{\mathrm{K}}} - \overbrace{\overline{g_{\mathrm{Na}}m^{3}}h(V - E_{\mathrm{Na}})}^{I_{\mathrm{Na}}} - \overbrace{\overline{g_{\mathrm{L}}(V - E_{\mathrm{L}})}}^{I_{\mathrm{L}}}$$

$$\dot{n} = \alpha_{n}(V)(1 - n) - \beta_{n}(V)n$$

$$\dot{m} = \alpha_{m}(V)(1 - m) - \beta_{m}(V)m$$

$$\dot{h} = \alpha_{h}(V)(1 - h) - \beta_{h}(V)h ,$$

$$\begin{aligned} \alpha_n(V) &= 0.01 \frac{10 - V}{\exp(\frac{10 - V}{10}) - 1} ,\\ \beta_n(V) &= 0.125 \exp\left(\frac{-V}{80}\right) ,\\ \alpha_m(V) &= 0.1 \frac{25 - V}{\exp(\frac{25 - V}{10}) - 1} ,\\ \beta_m(V) &= 4 \exp\left(\frac{-V}{18}\right) ,\\ \alpha_h(V) &= 0.07 \exp\left(\frac{-V}{20}\right) ,\\ \beta_h(V) &= \frac{1}{\exp(\frac{30 - V}{10}) + 1} .\end{aligned}$$



Dynamical Systems



Types of dynamical systems:

Differential equations

$$C\dot{V} = I - \overbrace{\bar{g}_{\mathrm{K}}n^{4}(V-E_{\mathrm{K}})}^{I_{\mathrm{K}}} - \overbrace{\bar{g}_{\mathrm{Na}}m^{3}h(V-E_{\mathrm{Na}})}^{I_{\mathrm{Na}}} - \overbrace{g_{\mathrm{L}}(V-E_{\mathrm{L}})}^{I_{\mathrm{L}}}$$

$$\dot{n} = \alpha_{n}(V)(1-n) - \beta_{n}(V)n$$

$$\dot{m} = \alpha_{m}(V)(1-m) - \beta_{m}(V)m$$

$$\dot{h} = \alpha_{h}(V)(1-h) - \beta_{h}(V)h ,$$

Logistic map

Maps

$$x_{n+1}=rx_n(1-x_n)$$

where x_n is a number between 0 and 1, which represents the ratio of existing population to the maximum possible population







The power of the dynamical systems approach to neuroscience (and to many other sciences) is that we can tell many things about a system without knowing all the details that govern the system evolution.



Phase portraits

Quiescent neuron whose membrane potential is resting

 $\underbrace{\widehat{E}}_{\underline{2}}$ (a) resting





Isn't it amazing that we can reach such a conclusion without knowing the equations that describe the neuron's dynamics?

We do not even know the number of variables needed to describe the neuron





Neuron in an excitable mode



Quiescent neuron whose

Small perturbations **(A)** result in small excursions from the equilibrium (**PSP**, postsynaptic potential).

Larger perturbations **(B)**, are amplified by the neuron's intrinsic dynamics and result in the **spike response**.







Quiescent neuron whose Neuron in an excitable mode Pacemaker neuron membrane potential is resting (a) resting (b) excitable (c) periodic spiking membrane potential, V(t) spike PSP PSP time, t В А stimulus stimuli gate, Phase portrait Stable equilibrium periodic spike activation orbit PSP equilibrium AΒ + ¥ membrane potential, V



Equilibria and limit cycles can coexist, so a neuron can be switched from one mode to another by a transient input







Qualitative changes

What is a bifurcation?



Bifurcations

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Quiescent neuron whose Neuron in an excitable mode **Qualitative changes** membrane potential is resting (a) resting V(t) (b) excitable If the dynamical system membrane potential, goes from (a) to (b), spike is it going through a bifurcation? PSP PSP No bifurcation! time, t B Α stimulus stimuli gate, This dynamical system contains (a) Stable equilibrium The differences between spike activation (A) and (B) are the initial **PSP** equilibrium conditions. A B There is not a +⊻ qualitative change membrane potential, V



Neuron in an excitable mode



If the dynamical system goes from **(b)** to **(c)**, is it going through a bifurcation?

Let's see... (b) : stable fix point (c) : unstable fix point and a limit cycle.

There is a qualitative change

Bifurcation!

(b) excitable spike PSP Α stimuli spike PSP ΑΒ

Pacemaker neuron

(c) periodic spiking











As the magnitude of the injected current slowly increases, the neurons bifurcate from resting (equilibrium) mode to tonic spiking (limit cycle) mode.





Equilibrium state leading to the transition from **resting** to **periodic spiking** behavior in neurons. (codimension-1, i.e., 1 control parameter)



Saddle-node bifurcation

Depending on the initial conditions, the neuron may spike (or decay to the stable resting position) or burst

Bifurcation point

The saddle and node colapse and annihilate each other. Only the limit cycle survives





Equilibrium state leading to the transition from **resting** to **periodic spiking** behavior in neurons. (codimension-1, i.e., 1 control parameter)















Saddle-node on invariant circle bifurcation









Saddle-node on invariant circle bifurcation





Equilibrium state leading to the transition from **resting** to **periodic spiking** behavior in neurons. (codimension-1, i.e., 1 control parameter)



As the magnitude of the injected current increases, the amplitude of the limit cycle increases, and it becomes a full-size spiking limit cycle





Equilibrium state leading to the transition from **resting** to **periodic spiking** behavior in neurons.



The stable equilibrium loses stability and gives birth to a small-amplitude limit cycle attractor



coexistence of resting and spiking states YES NO (bistable) (monostable) subthreshold oscillations (integrator) saddle-node on **N** saddle-node invariant circle (resonator) subcritical YES supercritical Andronov-Hopf Andronov-Hopf











Building models



First of all: you need neural recordings! (from your own experiments or from a collaborator)

To make a model of a neuron: put the right kind of currents together and tune the parameters so that the model can fire spikes like the ones recorded.

Another way is to determine what kind of bifurcations the neuron undergoes and how the bifurcations depend on neuromodulators and pharmacological blockers.

These approaches can be complementary.

Interdisciplinary work

Respect the different "ideologies"



The Hodgkin – Huxley model

Using **pioneering experimental techniques** of that time, Hodgkin and Huxley (1952) determined that the squid axon carries three major currents:

- Voltage-gated persistent K^+ current with four activation gates (resulting in the term n^4 in the equation below, where n is the activation variable for K^+);
- Voltage-gated transient Na⁺ current with three activation gates and one inactivation gate (the term m³h below)
- Ohmic leak current, I_L , which is carried mostly by Cl^{-} ions. $\begin{aligned}
 \alpha_n(V) &= 0.01 \frac{10-V}{\exp(\frac{10-V}{10})-1}, \\
 \alpha_n(V) &= 0.125 \exp\left(\frac{-V}{80}\right), \\
 \beta_n(V) &= 0.125 \exp\left(\frac{-V}{80}\right), \\
 \beta_n(V) &= 0.125 \exp\left(\frac{-V}{80}\right), \\
 \alpha_m(V) &= 0.1 \frac{25-V}{\exp(\frac{25-V}{10})-1}, \\
 \dot{m} &= \alpha_n(V)(1-m) - \beta_n(V)m \\
 \dot{h} &= \alpha_h(V)(1-h) - \beta_h(V)h, \\
 \dot{n} &= 0.01 \frac{10-V}{\exp(\frac{10-V}{10})-1}, \\
 \beta_n(V) &= 0.125 \exp\left(\frac{-V}{80}\right), \\
 \beta_m(V) &= 4 \exp\left(\frac{-V}{18}\right), \\
 \alpha_h(V) &= 0.07 \exp\left(\frac{-V}{20}\right), \\
 \dot{n} &= 0.01 \frac{10-V}{\exp(\frac{10-V}{10})-1}, \\
 \dot{n} &= 0.01 \frac{10-V}{\exp(\frac{10-V}{10}-1}, \\
 \dot{n} &= 0.01 \frac{10-V}{10}, \\
 \dot{n} &= 0$

$$\alpha_h(V) = 0.07 \exp\left(\frac{-V}{20}\right) ,$$

$$\beta_h(V) = \frac{1}{\exp(\frac{30-V}{10}) + 1} .$$



The Hodgkin – Huxley model

Using **pioneering experimental techniques** of that time, Hodgkin and Huxley (1952) determined not only the equations but **measured all the parameters values** :

$$C\dot{V} = I - \overbrace{\bar{g}_{\mathrm{K}}n^{4}(V-E_{\mathrm{K}})}^{I_{\mathrm{K}}} - \overbrace{\bar{g}_{\mathrm{Na}}m^{3}h(V-E_{\mathrm{Na}})}^{I_{\mathrm{Na}}} - \overbrace{g_{\mathrm{L}}(V-E_{\mathrm{L}})}^{I_{\mathrm{L}}} \qquad \alpha_{n}(V)$$

$$\dot{n} = \alpha_{n}(V)(1-n) - \beta_{n}(V)n$$

$$\dot{m} = \alpha_{m}(V)(1-m) - \beta_{m}(V)m$$

$$\dot{h} = \alpha_{h}(V)(1-h) - \beta_{h}(V)h, \qquad \alpha_{m}(V)$$

Values of shifted Nernst equilibrium potentials (so that $V_{rest} = 0$):

 $E_{\rm K} = -12 \ {\rm mV} \;, \qquad E_{\rm Na} = 120 \ {\rm mV} \;, \qquad E_{\rm L} = 10.6 \ {\rm mV};$

Values of maximal conductances: $\bar{g}_{\rm K} = 36 \ {
m mS/cm}^2$, $\bar{g}_{\rm Na} = 120 \ {
m mS/cm}^2$, $g_{\rm L} = 0.3 \ {
m mS/cm}^2$.

Value of membrane capacitance:

 $C=1\,\mu\mathrm{F}/\mathrm{cm}^2$

$$\alpha_n(V) = 0.01 \frac{10 - V}{\exp(\frac{10 - V}{10}) - 1},$$

$$\beta_n(V) = 0.125 \exp\left(\frac{-V}{80}\right),$$

$$\alpha_m(V) = 0.1 \frac{25 - V}{\exp(\frac{25 - V}{10}) - 1},$$

$$\beta_m(V) = 4 \exp\left(\frac{-V}{18}\right),$$

$$\alpha_h(V) = 0.07 \exp\left(\frac{-V}{20}\right),$$

$$\beta_h(V) = \frac{1}{\exp(\frac{30 - V}{10}) + 1}.$$

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The Hodgkin – Huxley model

The functions $\alpha(V)$ and $\beta(V)$ describe the transition rates between open and closed states of the channels

The notation presented before was used only for historical reasons. It is more convenient to use:

$$\dot{n} = (n_{\infty}(V) - n)/\tau_n(V) ,$$

$$\dot{m} = (m_{\infty}(V) - m)/\tau_m(V) ,$$

$$\dot{h} = (h_{\infty}(V) - h)/\tau_h(V) ,$$

where

$$n_{\infty} = \alpha_n / (\alpha_n + \beta_n) , \qquad \tau_n = 1 / (\alpha_n + \beta_n) , m_{\infty} = \alpha_m / (\alpha_m + \beta_m) , \qquad \tau_m = 1 / (\alpha_m + \beta_m) , h_{\infty} = \alpha_h / (\alpha_h + \beta_h) , \qquad \tau_h = 1 / (\alpha_h + \beta_h)$$







The Hodgkin – Huxley model





To be continued...

