



# Ana Amador

(she / her)

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ARGENTINA

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# Ana Amador

Interdisciplinary work in neuroscience

Masters in Physics, PhD in Physics (interdisciplinary) @ Univ. of Buenos Aires

Postdoc in Neuroscience (Organismal Biol & Anatomy) @ University of Chicago

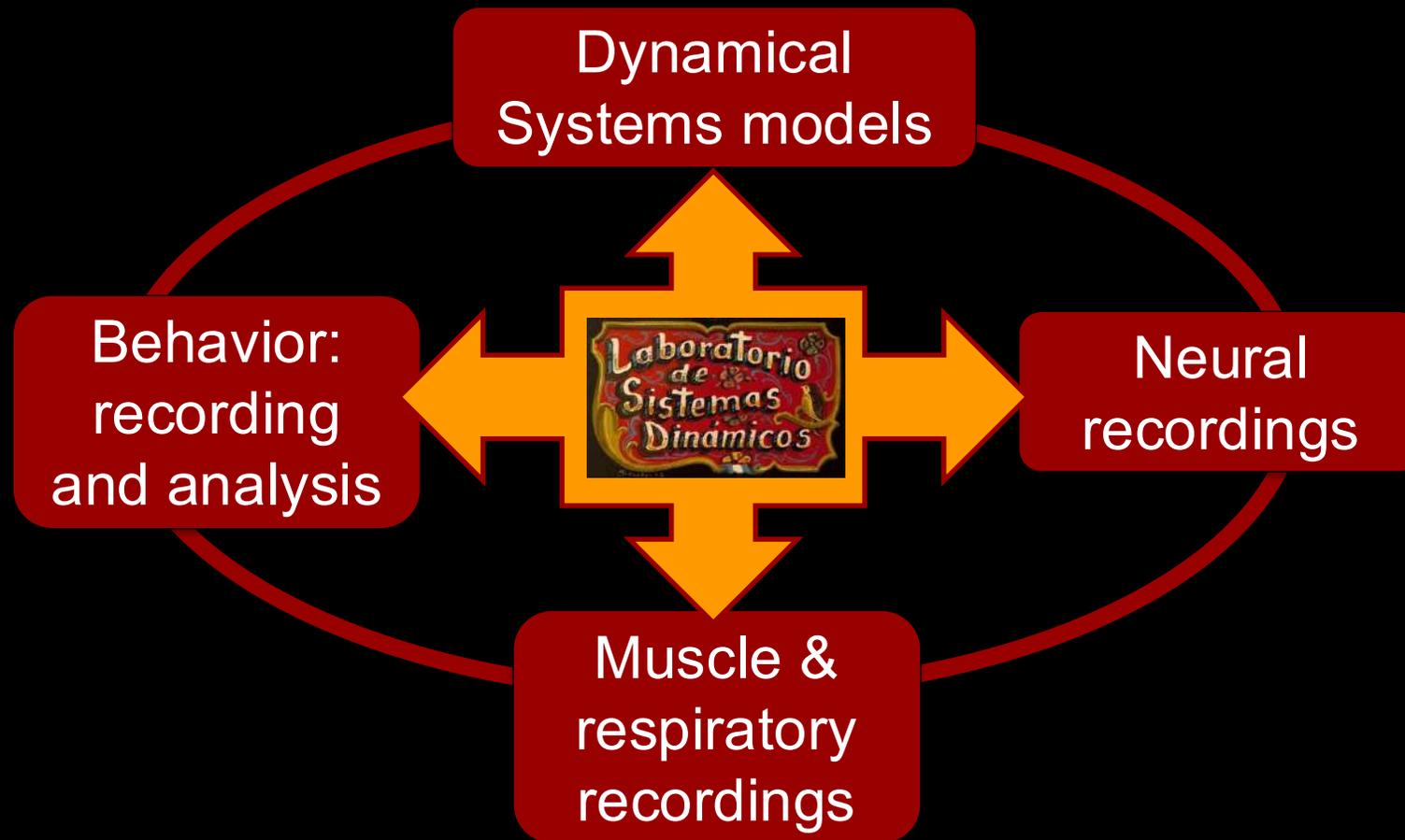
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The goal of our research is to shed light on the **dynamical mechanisms involved in the perception and the generation of complex sounds** and to study the brain and the peripheral system in this process.





## Lecture 1

Complex Systems in the modern era.

Nonlinear dynamics and excitable systems: from neurons to birdsong.

## Lecture 2

Dynamical models, neurons and experimental data.

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# Lecture 1

## Ana Amador

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One of the crucial intellectual decisions facing young scientists today is determining the balance between **interpretable** and **data-driven** approaches when addressing a scientific problem.



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### **Interpretable science**

Variables have meaning

The relationship between the variables are interpretable mechanisms

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### **Interpretable science**

Variables have meaning

The relationship between the variables are interpretable mechanisms

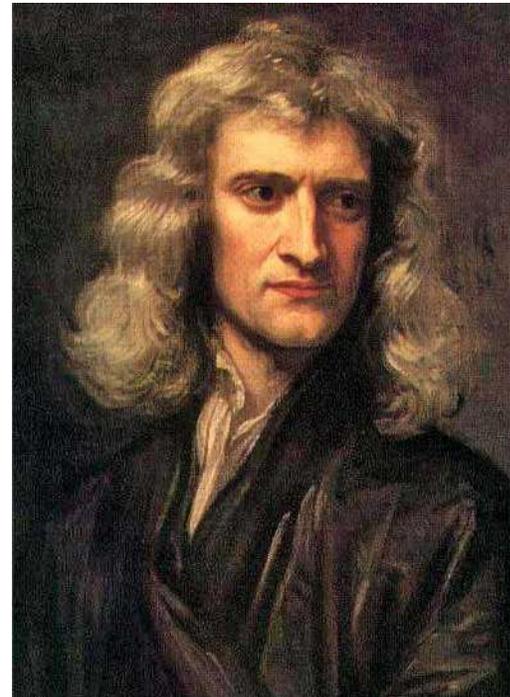
### **Data driven science**

A complex "non interpretable" model (as a neural network) is trained with examples, and the model does not share with us the rationale behind its success

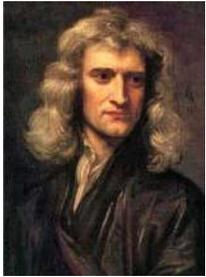
## Counterpoint with history



Kepler (1571-1630)



Newton (1643-1727))



Laplace (1749-1827): this is the “world’s system”  
All we have to do is to compute “f”, and the initial conditions

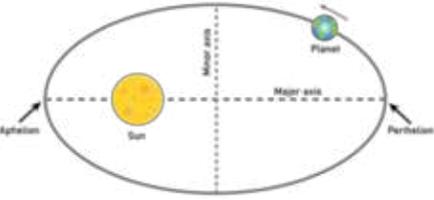
Why should we try to describe a problem with differential equations?  
Should we? Can we?

One of the biggest revolutions in science was data driven.  
And the “conversation” between Kepler and Newton is  
the first battle between data science and interpretable science

### Kepler's Laws

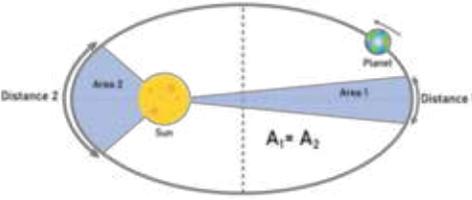
#### First Law

All planets move around the sun in elliptical orbits with the sun at one of the foci



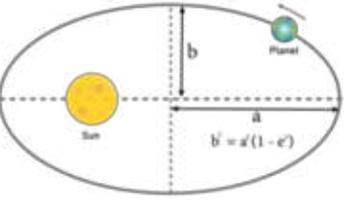
#### Second Law

A planet sweeps out equal areas in equal intervals of time



#### Third Law

The square of the orbital period of a planet is proportional to the cube of the orbit's semi-major axis



$T^2 \propto a^3$

T = Time to complete orbit  
a = Length of semi-major axis

The variables in Kepler's laws are interpretable, but we have no interpretable mechanism relating them.

# Newton's approach gave us more

We define the velocity.:  $\frac{dx}{dt} = v$

$$\frac{dv}{dt} = \begin{cases} 0 & \text{In the absence of interactions with the universe (Galileo)} \\ \frac{1}{m} & \text{Multiplied by a functional form describing the interaction} \end{cases}$$

Some functions, fundamental ones

$$\mathbf{F} = \frac{-G m M}{r_{12}^2} \mathbf{e}_{12}$$

Others, phenomenological

$$F = -kx$$

**To perform a prediction,  
we have to have a model relating  
the variables**

$$\frac{dx}{dt} = y$$

$$\frac{dy}{dt} = f(x, y)$$



# More than a law, it is a program of how to do science



1. Measure a finite set of initial conditions.
2. Elucidate the law that prescribes the rate of variation of these variables (assuming that the law involves the values of the variables **at that moment**).
3. Integrate an ODE

It does NOT describe

1. Systems of equations with delays
2. Partial differential equations (although...)

$$\frac{dx(t)}{dt} = x(t) - \sigma x(t - \tau)^2$$

Even electromagnetism is excluded...



# Dynamical Systems



**Definition** : set of **variables** that describe state of the system and a **law** that describes the evolution of the state variables with time

how the state of the system in the next moment of time depends on the input and its state in the previous moment of time

## Example:

### The Hodgkin-Huxley model

(4-dimensional dynamical system)

Its state is uniquely determined by the membrane potential,  $V$ , and the “gating variables”  $n$ ,  $m$ , and  $h$  for persistent  $K^+$  and transient  $Na^+$  currents.

The evolution law is given by a

**4-dimensional system of ordinary differential equations.**

$$\begin{aligned}
 C \dot{V} &= I - \overbrace{\bar{g}_K n^4 (V - E_K)}^{I_K} - \overbrace{\bar{g}_{Na} m^3 h (V - E_{Na})}^{I_{Na}} - \overbrace{g_L (V - E_L)}^{I_L} \\
 \dot{n} &= \alpha_n(V)(1 - n) - \beta_n(V)n \\
 \dot{m} &= \alpha_m(V)(1 - m) - \beta_m(V)m \\
 \dot{h} &= \alpha_h(V)(1 - h) - \beta_h(V)h,
 \end{aligned}$$

Is this dynamical system nonlinear?



# Nonlinear Dynamics



Nonlinear rules

Mechanisms responsible for governing the temporal evolution of a system

Let's see...

$$C\dot{V} = I - \overbrace{\bar{g}_K n^4 (V - E_K)}^{I_K} - \overbrace{\bar{g}_{Na} m^3 h (V - E_{Na})}^{I_{Na}} - \overbrace{g_L (V - E_L)}^{I_L}$$

$$\dot{n} = \alpha_n(V)(1 - n) - \beta_n(V)n$$

$$\dot{m} = \alpha_m(V)(1 - m) - \beta_m(V)m$$

$$\dot{h} = \alpha_h(V)(1 - h) - \beta_h(V)h,$$

$$\alpha_n(V) = 0.01 \frac{10 - V}{\exp(\frac{10-V}{10}) - 1},$$

$$\beta_n(V) = 0.125 \exp\left(\frac{-V}{80}\right),$$

$$\alpha_m(V) = 0.1 \frac{25 - V}{\exp(\frac{25-V}{10}) - 1},$$

$$\beta_m(V) = 4 \exp\left(\frac{-V}{18}\right),$$

$$\alpha_h(V) = 0.07 \exp\left(\frac{-V}{20}\right),$$

$$\beta_h(V) = \frac{1}{\exp(\frac{30-V}{10}) + 1}.$$



# Dynamical Systems



## Types of dynamical systems:

Differential equations

$$\begin{aligned} C \dot{V} &= I - \overbrace{\bar{g}_K n^4 (V - E_K)}^{I_K} - \overbrace{\bar{g}_{Na} m^3 h (V - E_{Na})}^{I_{Na}} - \overbrace{g_L (V - E_L)}^{I_L} \\ \dot{n} &= \alpha_n(V)(1 - n) - \beta_n(V)n \\ \dot{m} &= \alpha_m(V)(1 - m) - \beta_m(V)m \\ \dot{h} &= \alpha_h(V)(1 - h) - \beta_h(V)h, \end{aligned}$$

Maps

Logistic map

$$x_{n+1} = r x_n (1 - x_n)$$

where  $x_n$  is a number between 0 and 1, which represents the ratio of existing population to the maximum possible population

**Chaos!**



# Phase portraits



The power of the dynamical systems approach to neuroscience (and to many other sciences) is that we can tell many things about a system without knowing all the details that govern the system evolution.

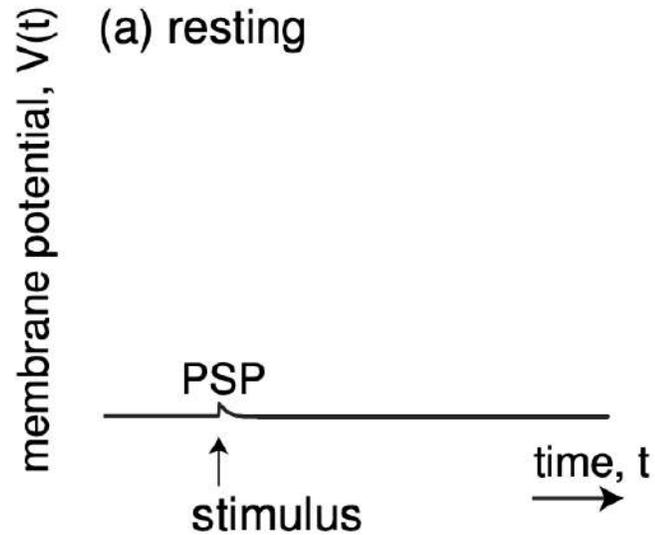


# Phase portraits



Quiescent neuron whose membrane potential is resting

(a) resting



Isn't it amazing that we can reach such a conclusion without knowing the equations that describe the neuron's dynamics?

**We do not even know the number of variables needed to describe the neuron**

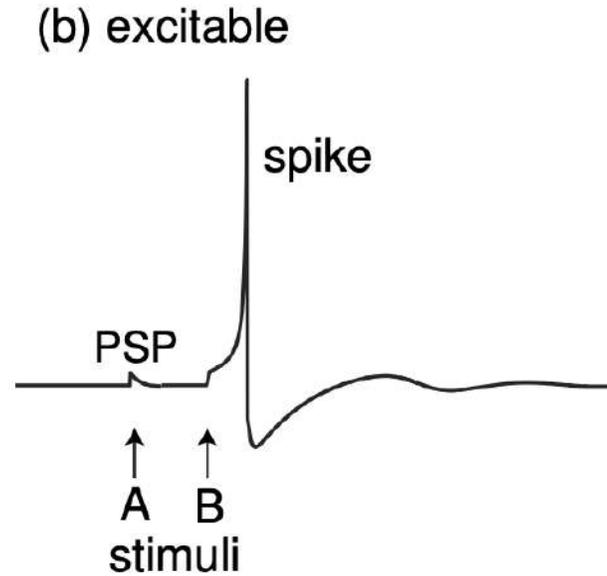
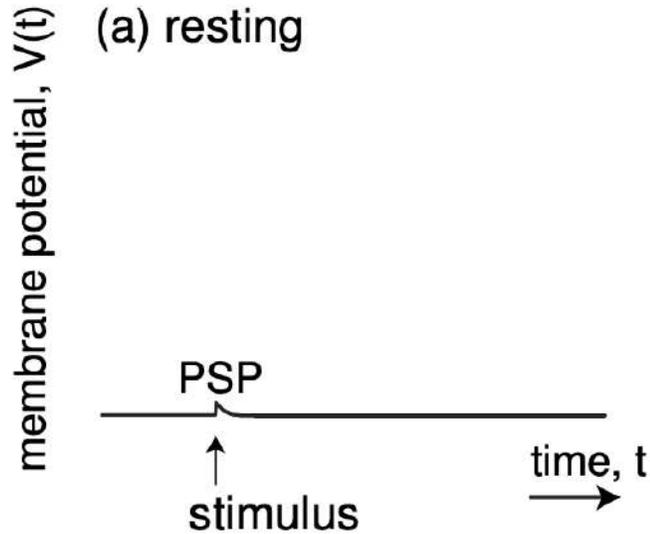


# Phase portraits



Quiescent neuron whose membrane potential is resting

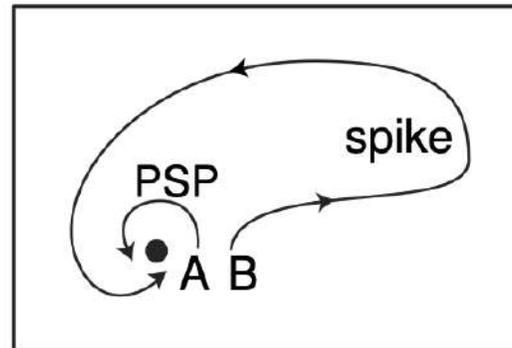
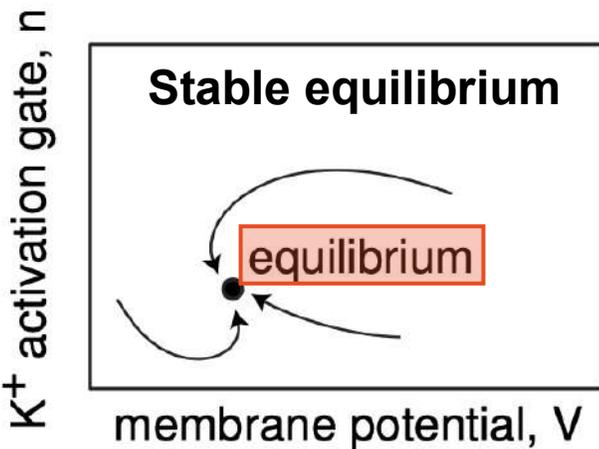
Neuron in an excitable mode



Small perturbations (**A**) result in small excursions from the equilibrium (**PSP**, postsynaptic potential).

Larger perturbations (**B**), are amplified by the neuron's intrinsic dynamics and result in the **spike response**.

Phase portrait



Excitable system

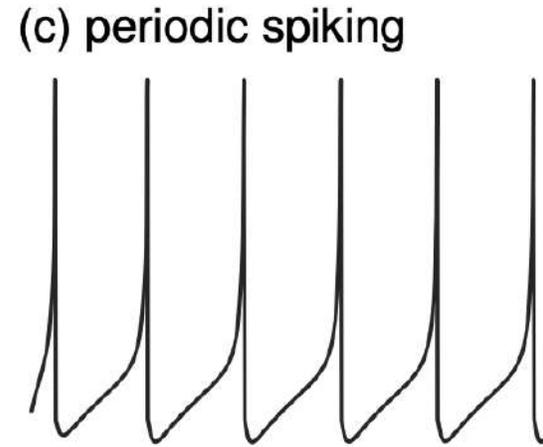
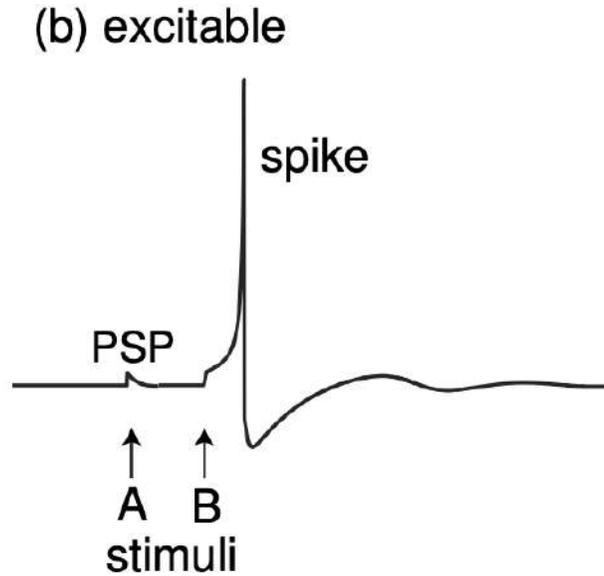
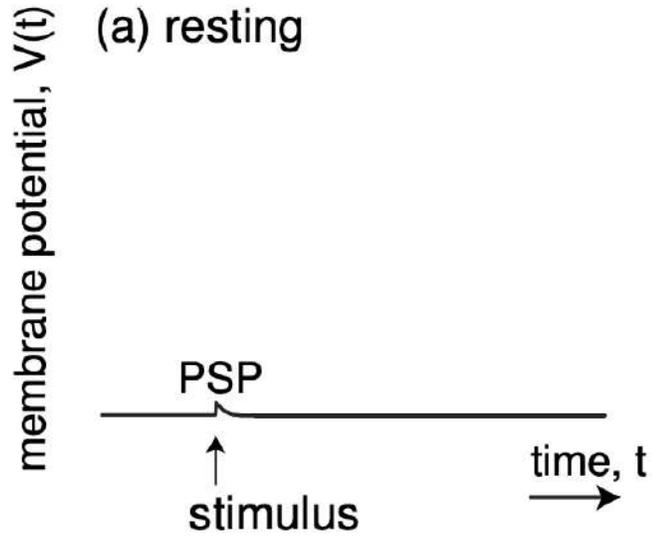
# Phase portraits



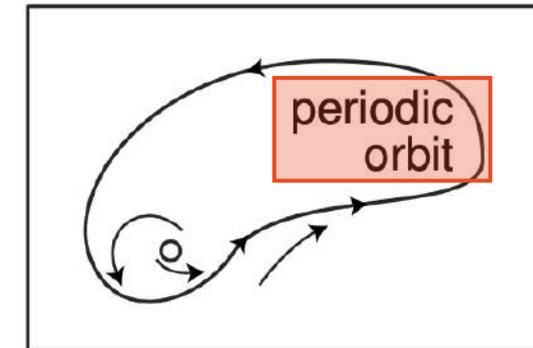
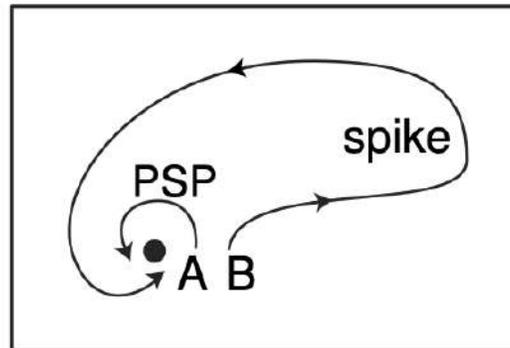
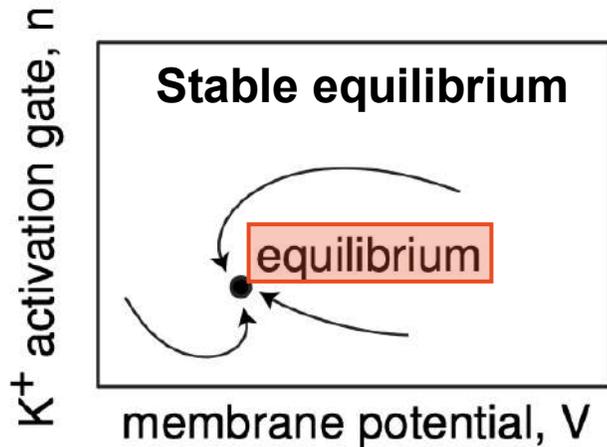
Quiescent neuron whose membrane potential is resting

Neuron in an excitable mode

Pacemaker neuron



Phase portrait

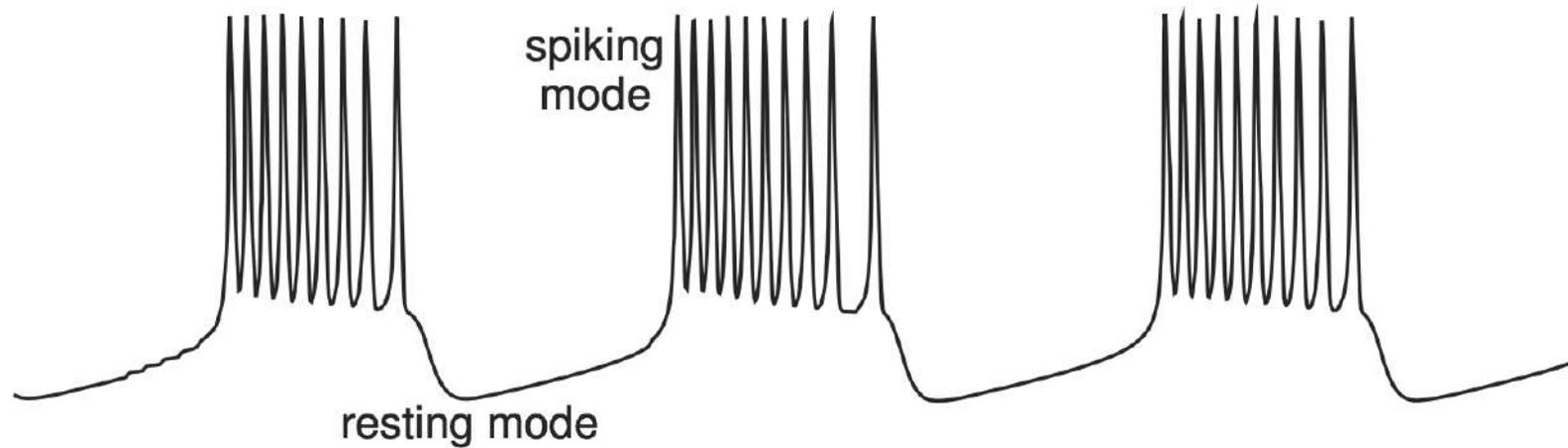




# Phase portraits

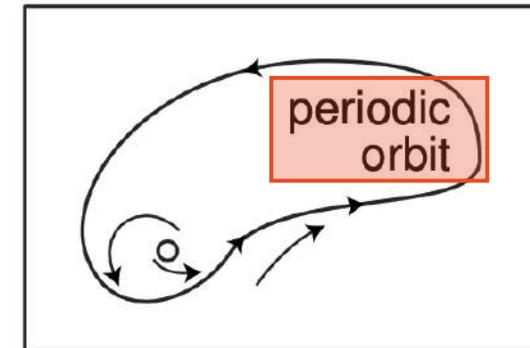
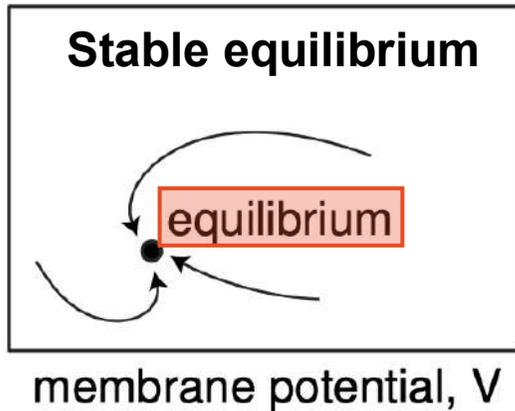


**Equilibria and limit cycles** can coexist, so a neuron can be switched from one mode to another by a transient input



Phase portrait

$K^+$  activation gate,  $n$





# Bifurcations



Qualitative changes

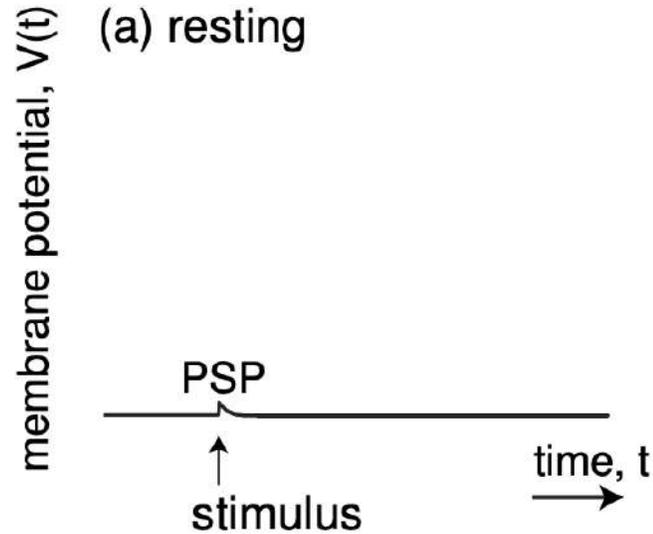
What is a bifurcation?



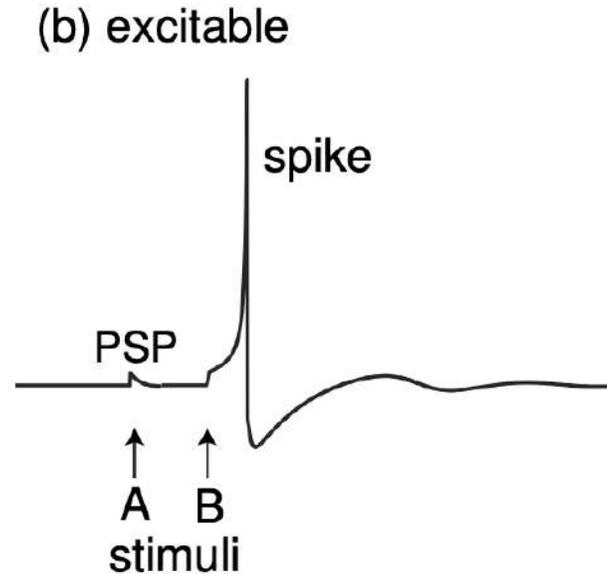
# Bifurcations



Quiescent neuron whose membrane potential is resting



Neuron in an excitable mode



Qualitative changes

If the dynamical system goes from (a) to (b), is it going through a bifurcation?

No bifurcation!

→ This dynamical system contains (a)  
The differences between (A) and (B) are the initial conditions.

There is not a qualitative change

# Bifurcations



If the dynamical system goes from **(b)** to **(c)**, is it going through a bifurcation?

Let's see...

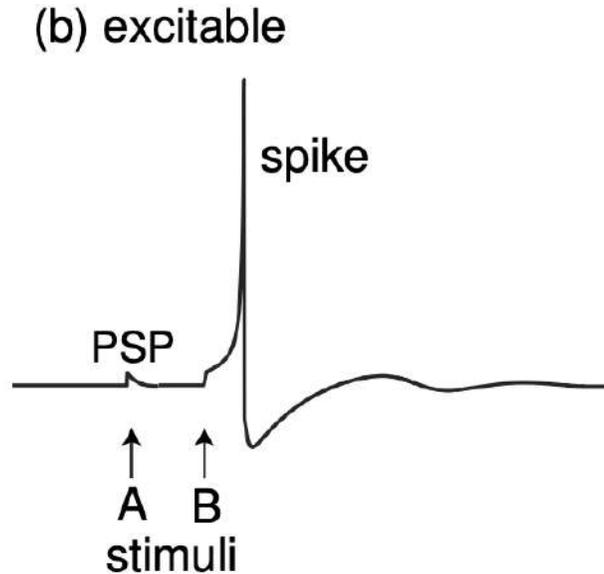
**(b)** : stable fix point

**(c)** : unstable fix point and a limit cycle.

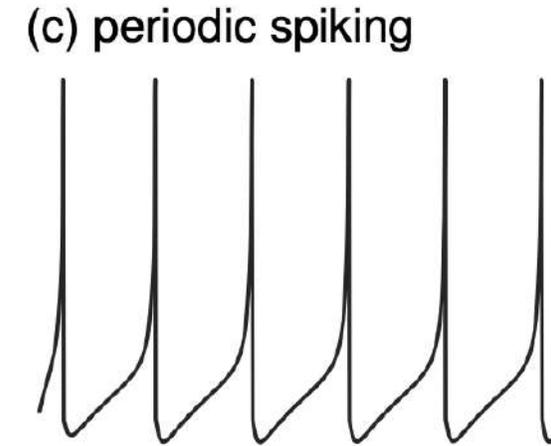
There is a **qualitative change**

**Bifurcation!**

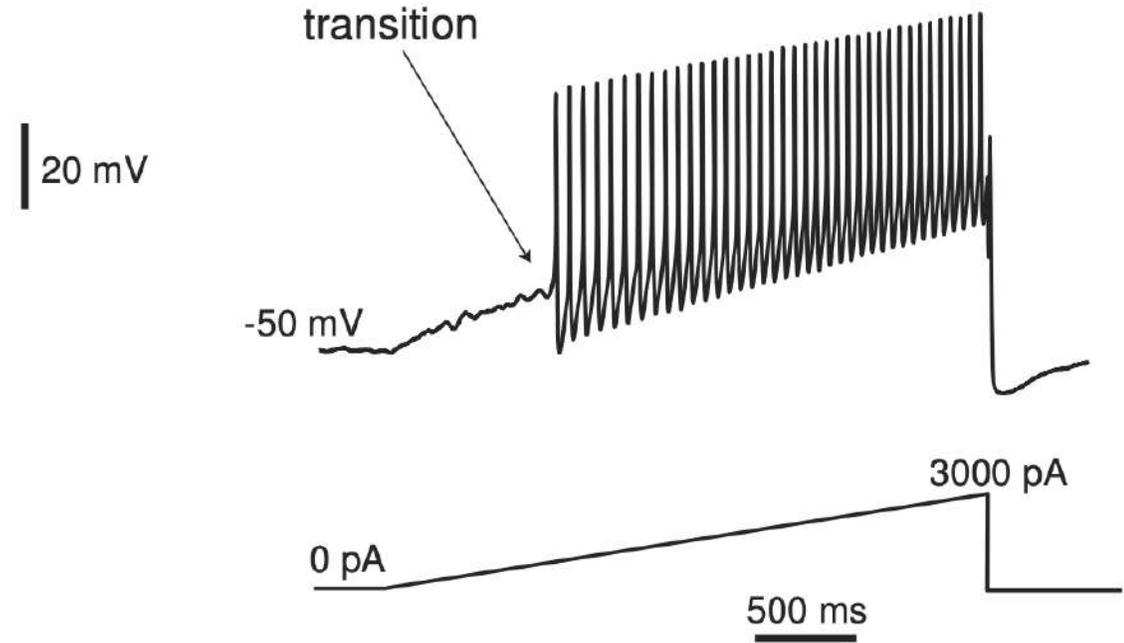
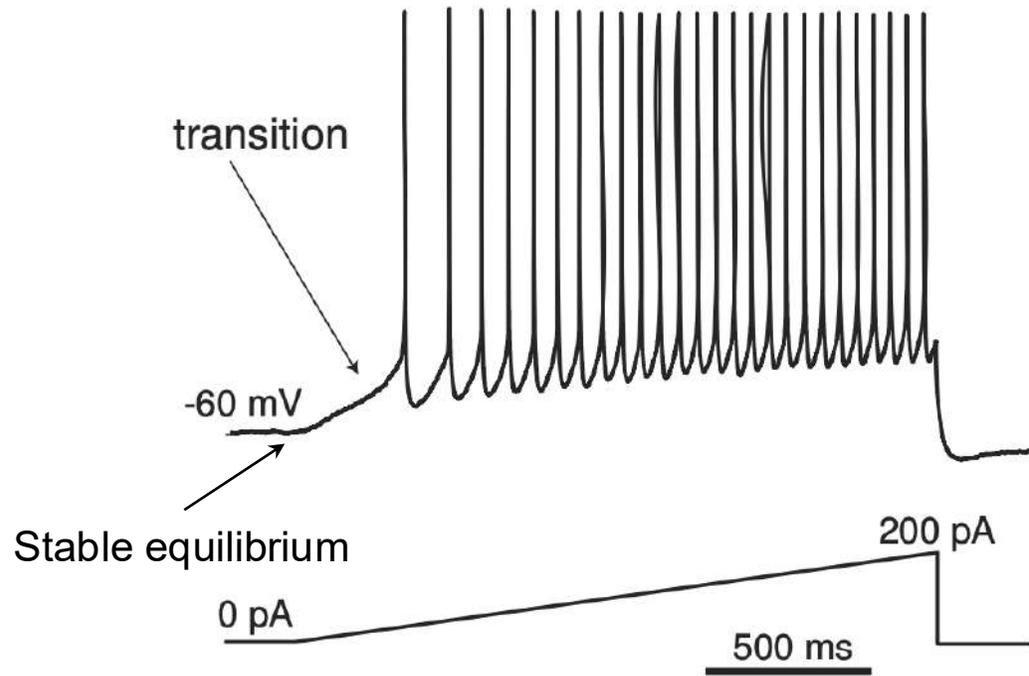
Neuron in an excitable mode



Pacemaker neuron



# Bifurcations

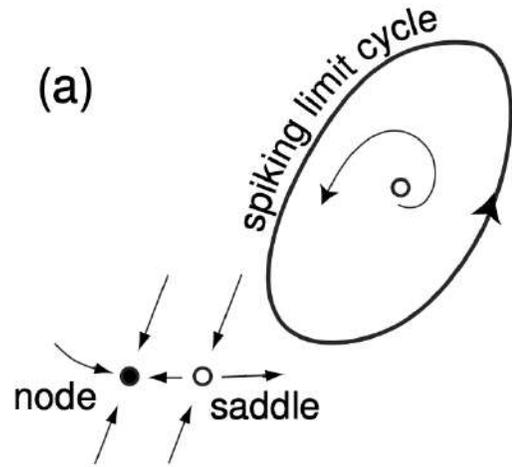


As the magnitude of the injected current slowly increases, the neurons bifurcate from resting (equilibrium) mode to tonic spiking (limit cycle) mode.

# Bifurcations



Equilibrium state leading to the transition from **resting** to **periodic spiking** behavior in neurons.  
(codimension-1, i.e., 1 control parameter)



**Saddle-node bifurcation**

Depending on the initial conditions, the neuron may spike (or decay to the stable resting position) or burst

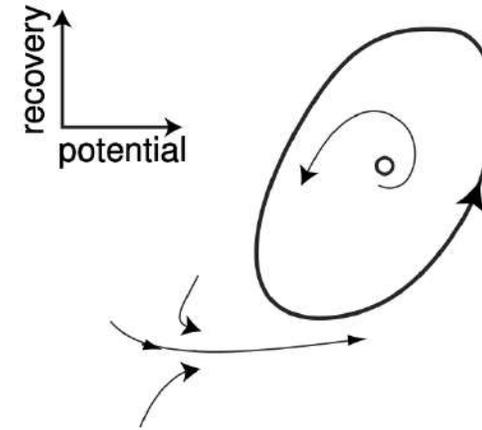
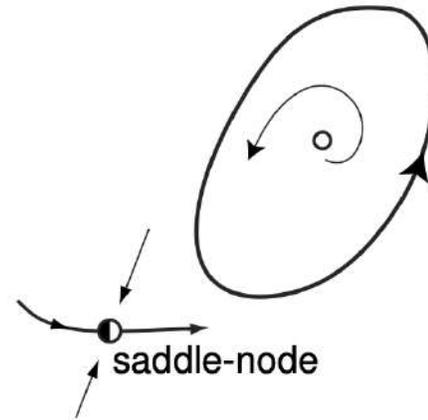
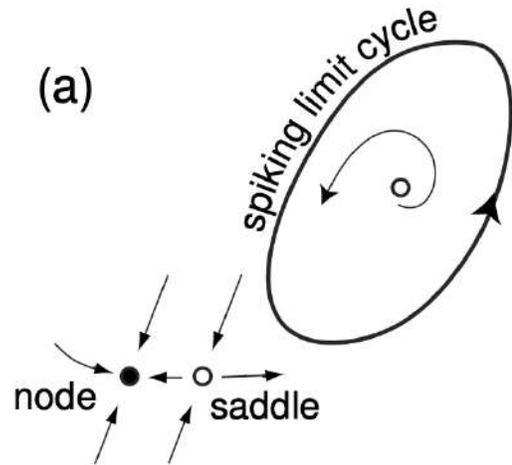
Bifurcation point

The saddle and node collapse and annihilate each other.  
Only the limit cycle survives

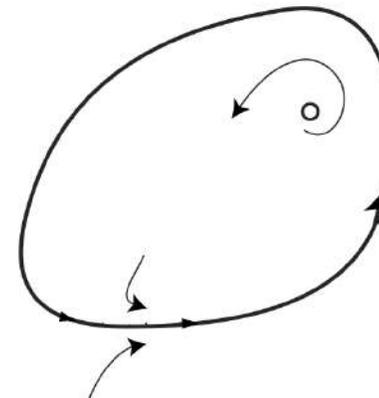
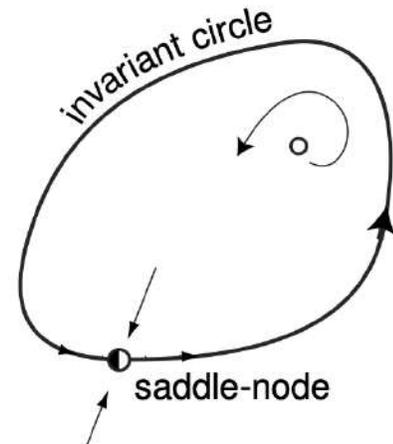
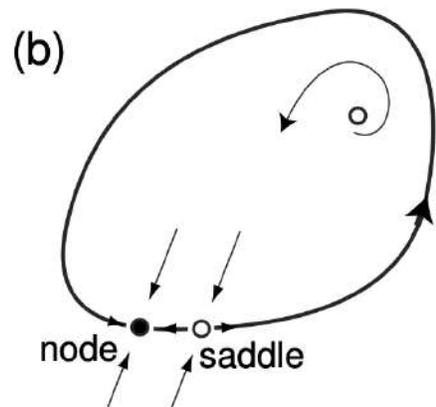
# Bifurcations



Equilibrium state leading to the transition from **resting** to **periodic spiking** behavior in neurons.  
(codimension-1, i.e., 1 control parameter)



**Saddle-node bifurcation**

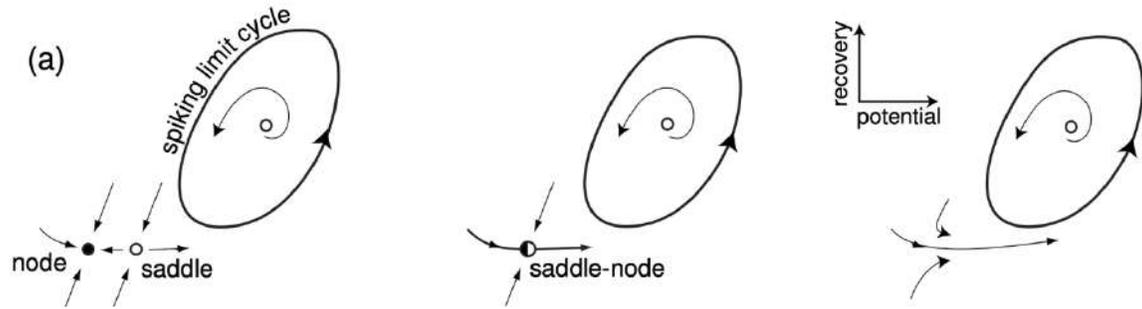


**Saddle-node on  
invariant circle  
bifurcation**

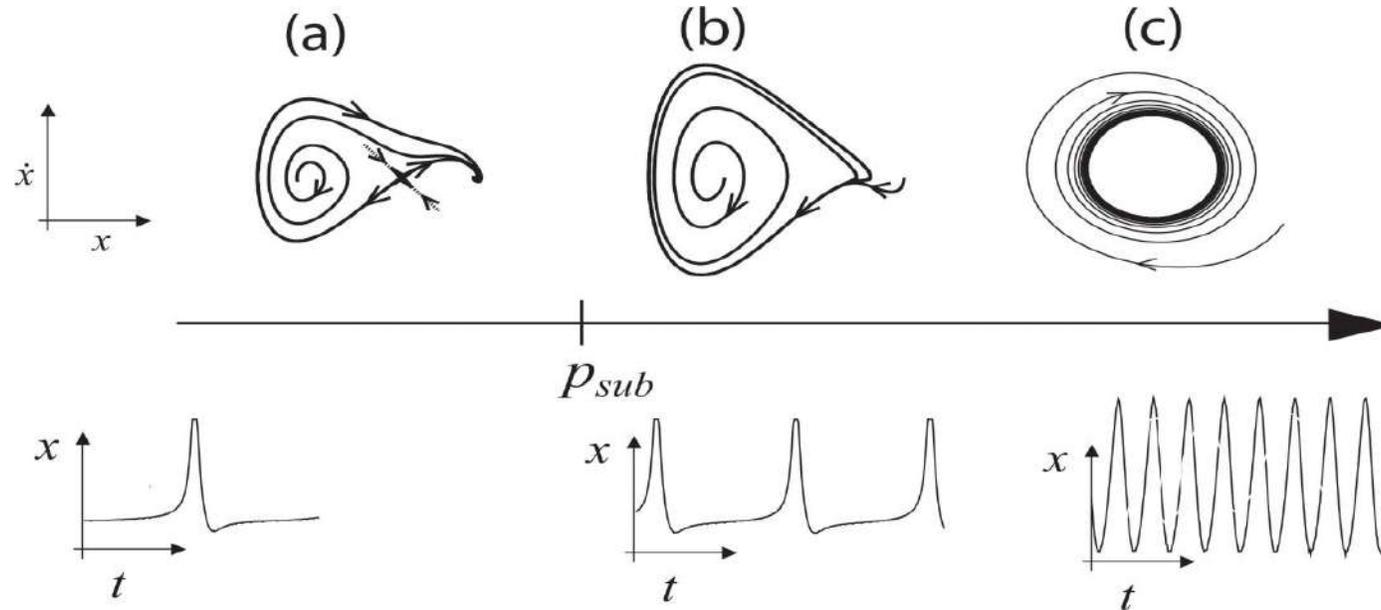
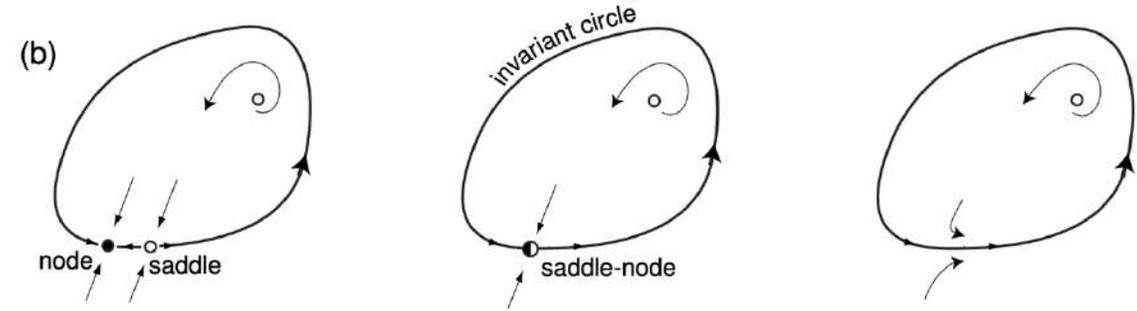
# Bifurcations



## Saddle-node bifurcation



## Saddle-node on invariant circle bifurcation



Saddle-node ghost

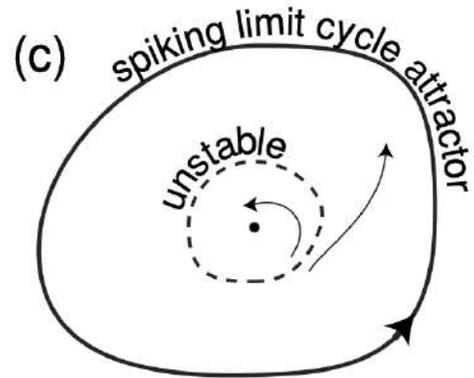
Saddle-node on invariant circle bifurcation



# Bifurcations



Equilibrium state leading to the transition from **resting** to **periodic spiking** behavior in neurons.  
(codimension-1, i.e., 1 control parameter)



**Subcritical Andronov-Hopf  
bifurcation**

A small unstable limit cycle shrinks to a stable equilibrium and makes it lose stability

The only stable state  
is the limit cycle

(d)



**Supercritical Andronov-Hopf  
bifurcation**

The stable equilibrium loses stability and gives birth to a small-amplitude limit cycle attractor

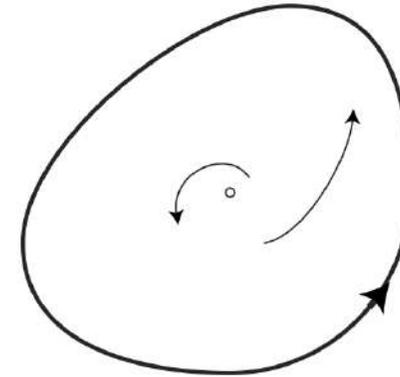
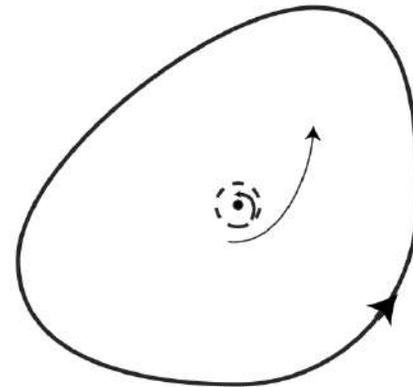
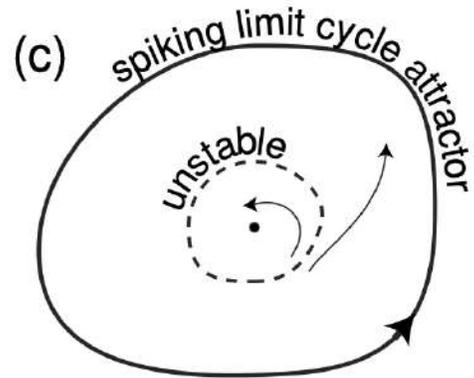
As the magnitude of the injected current increases, the amplitude of the limit cycle increases, and it becomes a full-size spiking limit cycle

# Bifurcations



Equilibrium state leading to the transition from **resting** to **periodic spiking** behavior in neurons.  
(codimension-1, i.e., 1 control parameter)

**Bi-stable**



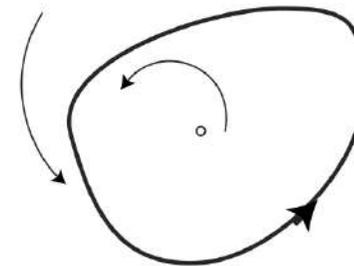
**Subcritical Andronov-Hopf bifurcation**

A small unstable limit cycle shrinks to a stable equilibrium and makes it lose stability

**The only stable state is the limit cycle**

(d)

**Mono-stable**



**Supercritical Andronov-Hopf bifurcation**

The stable equilibrium loses stability and gives birth to a small-amplitude limit cycle attractor



# Bifurcations



coexistence of resting and spiking states

YES  
(bistable)

NO  
(monostable)

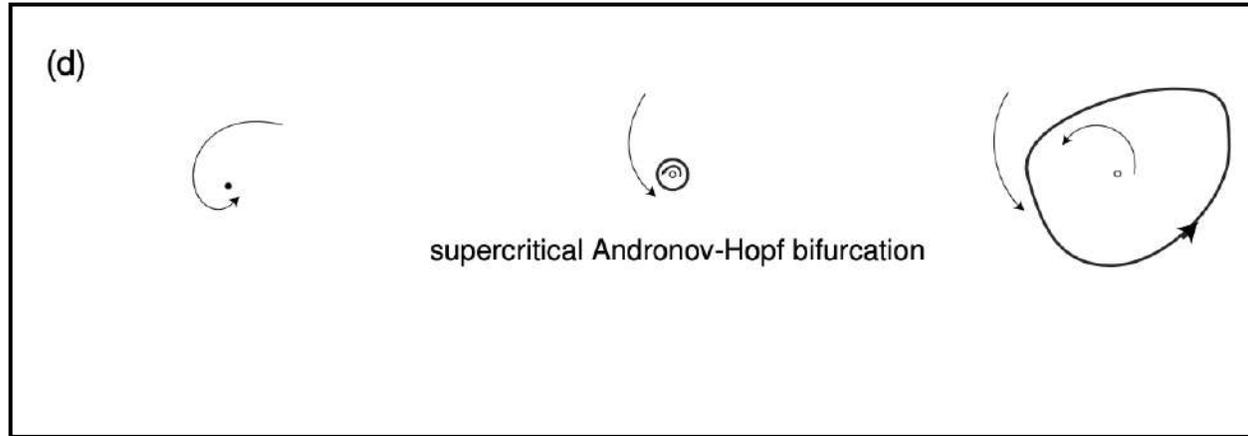
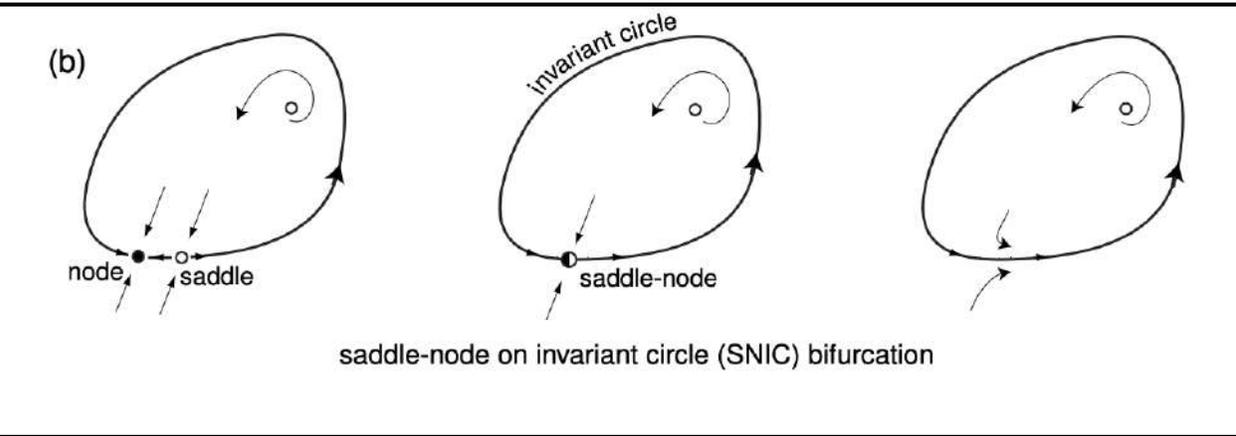
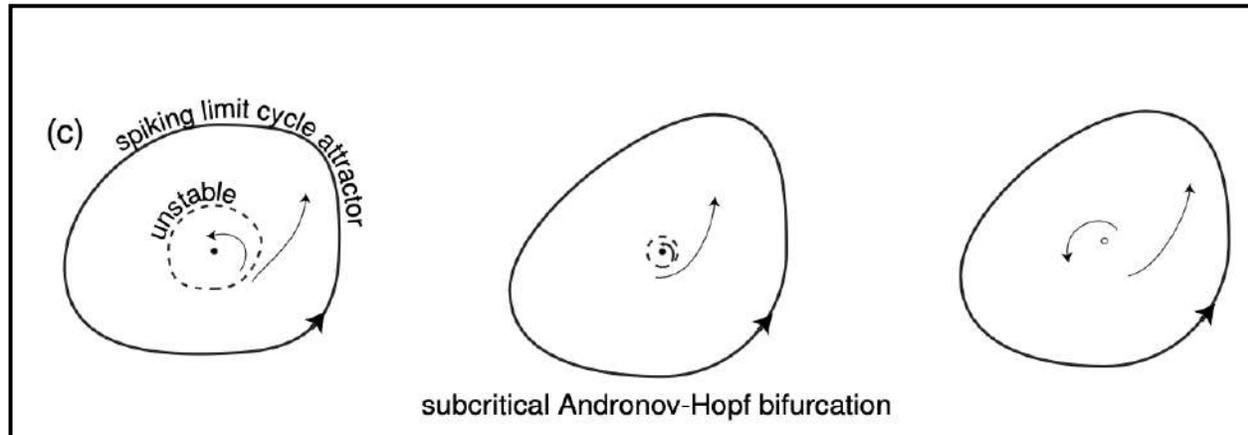
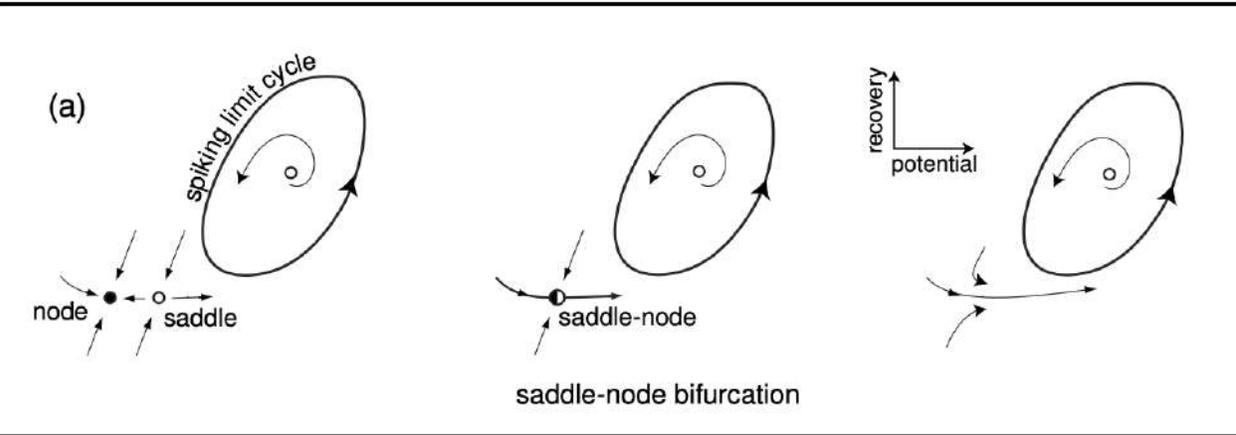
subthreshold oscillations

NO  
(integrator)

YES  
(resonator)

saddle-node	saddle-node on invariant circle
subcritical Andronov-Hopf	supercritical Andronov-Hopf

# Bifurcations





# Building models



First of all: you need neural recordings!  
(from your own experiments or from a collaborator)

To make a model of a neuron: put the right kind of currents together and tune the parameters so that the model can fire spikes like the ones recorded.

Another way is to determine what kind of bifurcations the neuron undergoes and how the bifurcations depend on neuromodulators and pharmacological blockers.

These approaches can be complementary.

Interdisciplinary work

Respect the different “ideologies”



# The Hodgkin – Huxley model



Using **pioneering experimental techniques** of that time, Hodgkin and Huxley (1952) determined that the squid axon carries three major currents:

- Voltage-gated persistent  $K^+$  current with four activation gates (resulting in the term  $n^4$  in the equation below, where  $n$  is the activation variable for  $K^+$ );
- Voltage-gated transient  $Na^+$  current with three activation gates and one inactivation gate (the term  $m^3h$  below)
- Ohmic leak current,  $I_L$ , which is carried mostly by  $Cl^-$  ions.

$$\begin{aligned}
 C \dot{V} &= I - \overbrace{\bar{g}_K n^4 (V - E_K)}^{I_K} - \overbrace{\bar{g}_{Na} m^3 h (V - E_{Na})}^{I_{Na}} - \overbrace{g_L (V - E_L)}^{I_L} \\
 \dot{n} &= \alpha_n(V)(1 - n) - \beta_n(V)n \\
 \dot{m} &= \alpha_m(V)(1 - m) - \beta_m(V)m \\
 \dot{h} &= \alpha_h(V)(1 - h) - \beta_h(V)h,
 \end{aligned}$$

$$\alpha_n(V) = 0.01 \frac{10 - V}{\exp\left(\frac{10 - V}{10}\right) - 1},$$

$$\beta_n(V) = 0.125 \exp\left(\frac{-V}{80}\right),$$

$$\alpha_m(V) = 0.1 \frac{25 - V}{\exp\left(\frac{25 - V}{10}\right) - 1},$$

$$\beta_m(V) = 4 \exp\left(\frac{-V}{18}\right),$$

$$\alpha_h(V) = 0.07 \exp\left(\frac{-V}{20}\right),$$

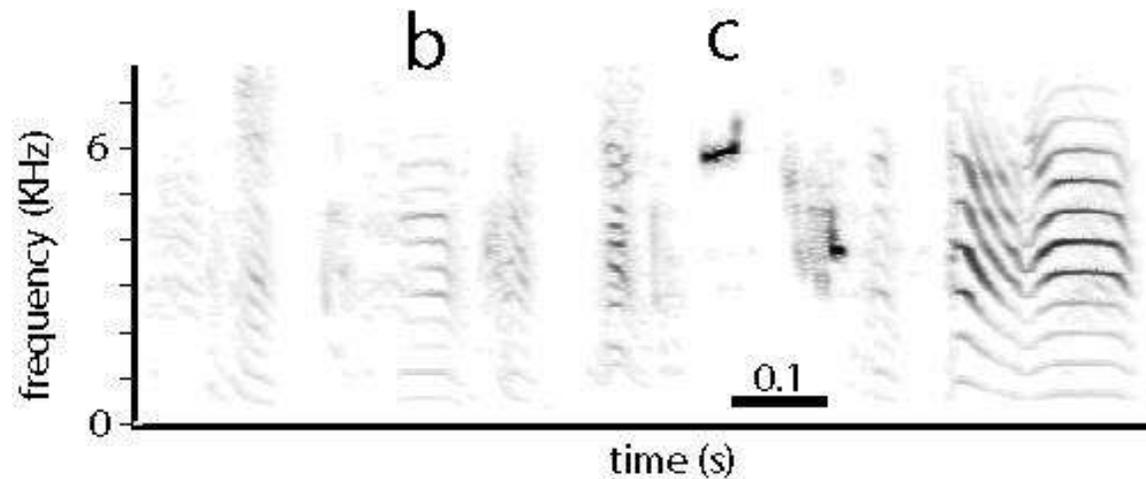
$$\beta_h(V) = \frac{1}{\exp\left(\frac{30 - V}{10}\right) + 1}.$$

This model predicted the existence of ion channels!

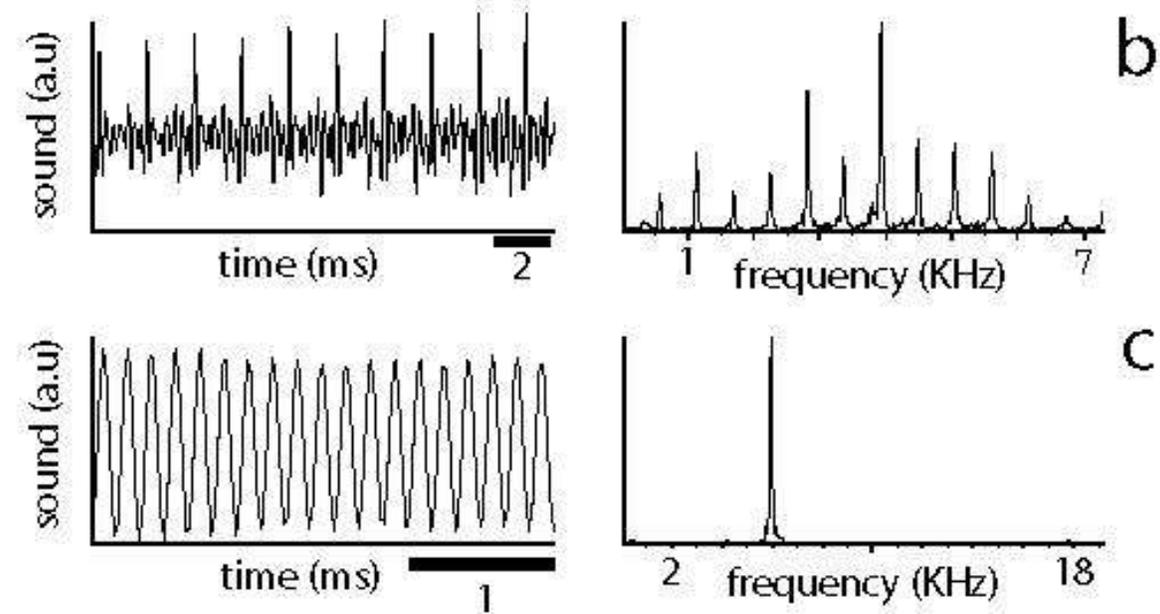


Let's see the power of physics and nonlinear dynamics!

# Birdsong as a complex mechanism



**Temporal trace:  
excitable system**



Spectrally rich

Almost tonal



# Birdsong as a complex mechanism

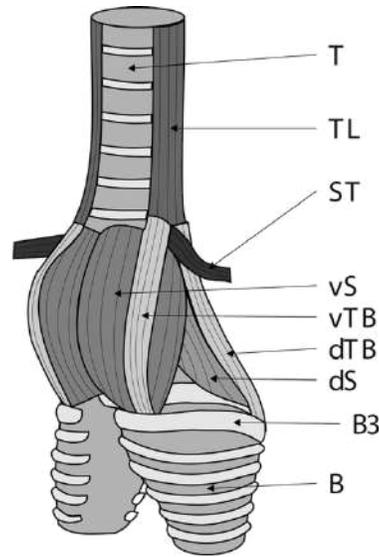
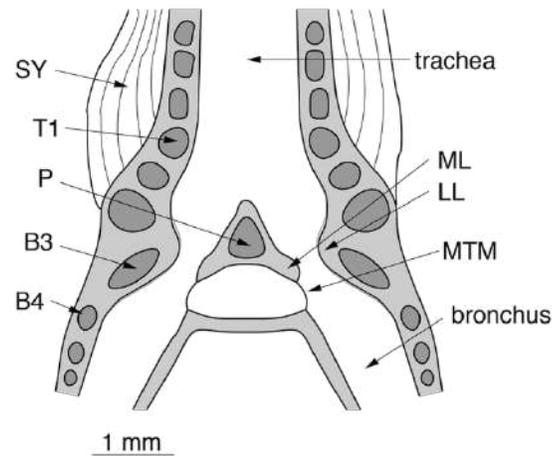


# When physics and biology meet...

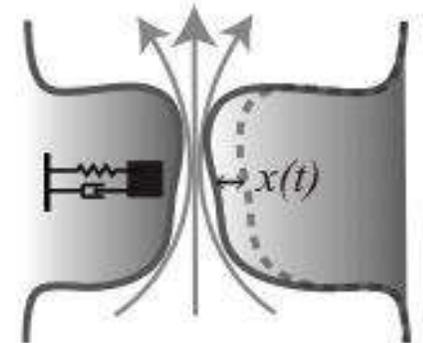
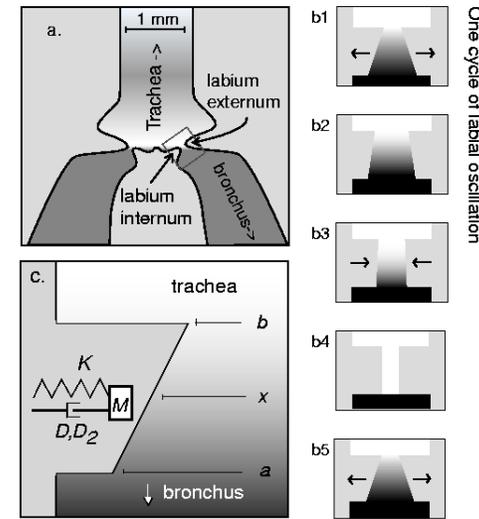


## Different views of the syrinx

- Biology is used to complexity



- Physics is obsessed with simplicity

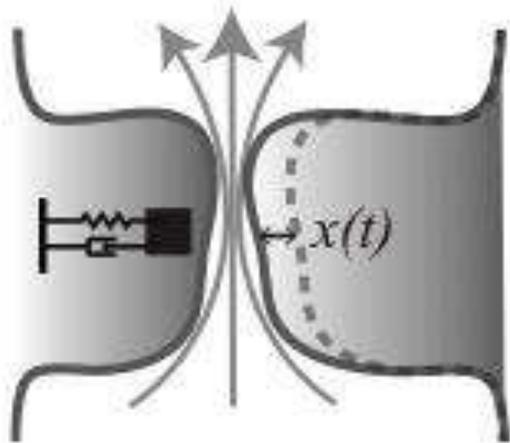




# The program of physics (or interpretable science)



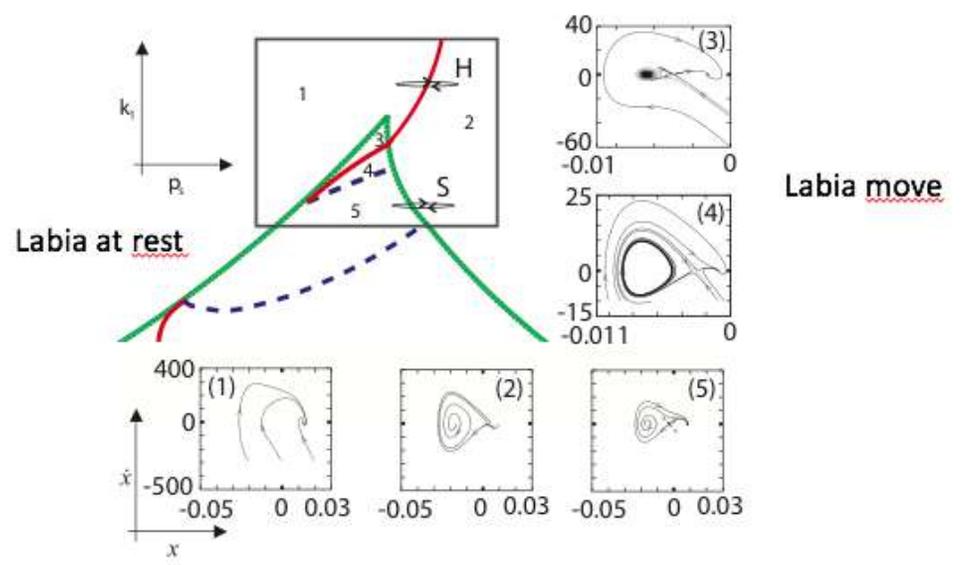
1. To identify the pertinent variables  
And how to relate them through a model



$$\left. \begin{aligned} \frac{dx}{dt} &= y, \\ \frac{dy}{dt} &= (1/m) \left[ -k(x)x - b(y)y - cx^2y + a_{lab}p_s \left( \frac{\Delta a + 2\tau y}{a_{01} + x + \tau y} \right) \right]. \end{aligned} \right\}$$

2. To study the solutions for different parameters

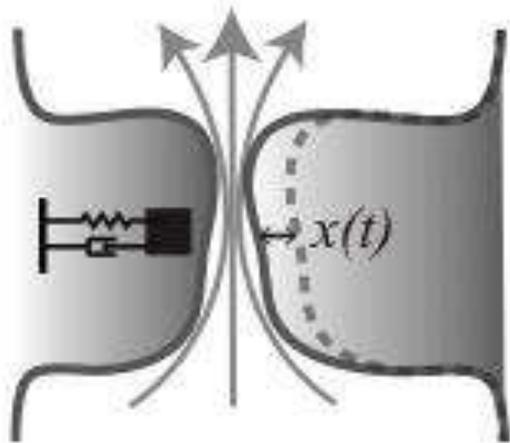
**Bifurcation diagram**





# The program of physics (or interpretable science)

1. To identify the pertinent variables  
And how to relate them through a model

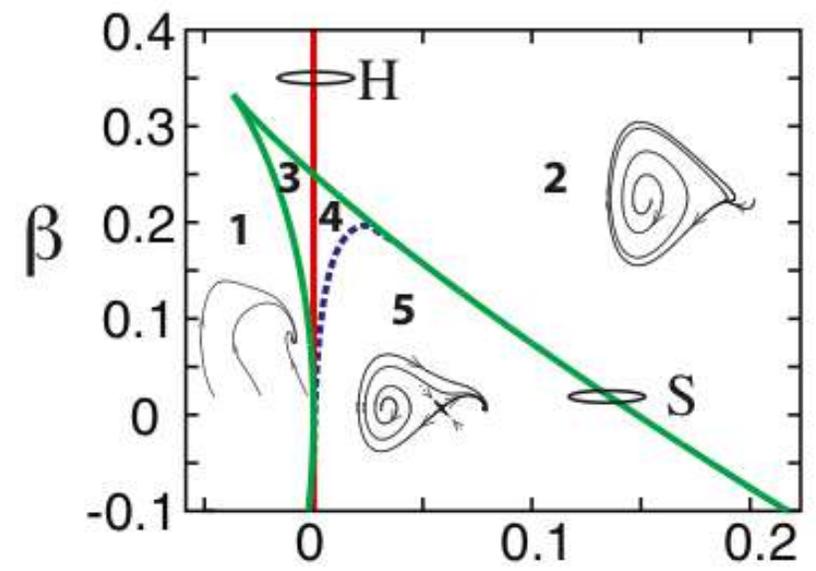


Normal form

$$\begin{cases} \frac{dx}{dt} = y \\ \frac{dy}{dt} = -\alpha(t)\gamma^2 - \beta(t)\gamma^2x - \gamma^2x^3 - \gamma x^2y + \gamma^2x^2 - \gamma xy \end{cases}$$

2. To study the solutions for different parameters

Bifurcation diagram



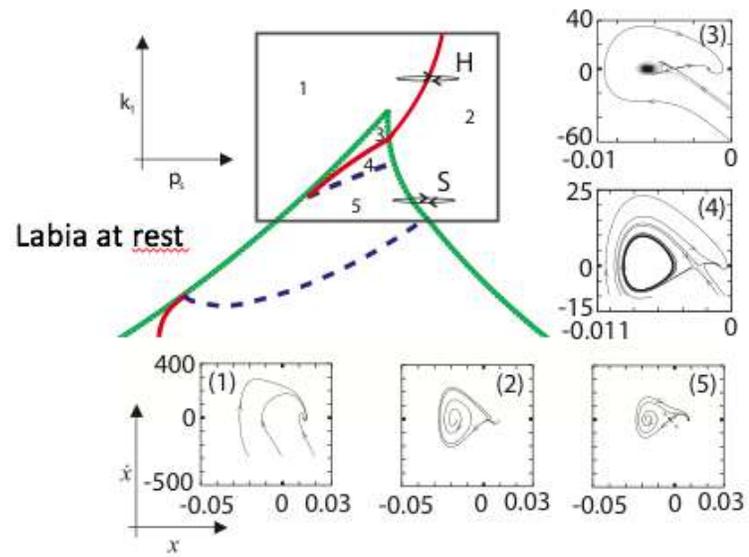
# Normal form reduction



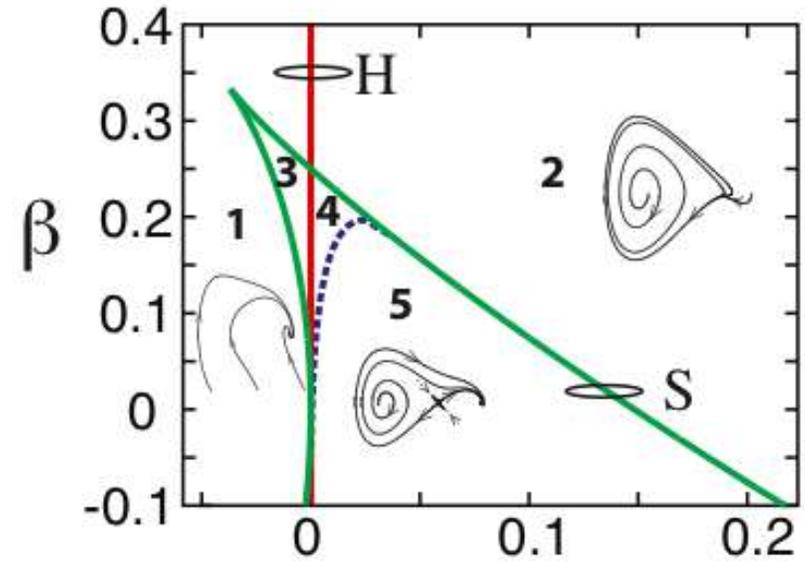

$$\left\{ \begin{array}{l} \frac{dx}{dt} = y, \\ \frac{dy}{dt} = (1/m) \left[ -k(x)x - b(y)y - cx^2y + a_{\text{lab}} p_s \left( \frac{\Delta a + 2\tau\tau}{a_{01} + x + \tau y} \right) \right]. \end{array} \right. \quad \left\{ \begin{array}{l} \frac{dx}{dt} = y \\ \frac{dy}{dt} = -\alpha(t)\gamma^2 - \beta(t)\gamma^2x - \gamma^2x^3 - \gamma x^2y + \gamma^2x^2 - \gamma xy \end{array} \right.$$

Algorithmic procedure that allows you to reduce your nonlinear problem to a simpler one, close to a linear singularity. This simpler model will have less parameters, and **has been probably studied**

# Normal form reduction



Labia move





# Dynamical analysis of the model



Parameters  $k_1$  y  $P_s$  are related to physiological variables:

$k_1 \propto$  activity of vS syringeal muscle

$P_s \propto$  subsyringeal pressure

## Bifurcations:

### H: Hopf:

✓ almost tonal

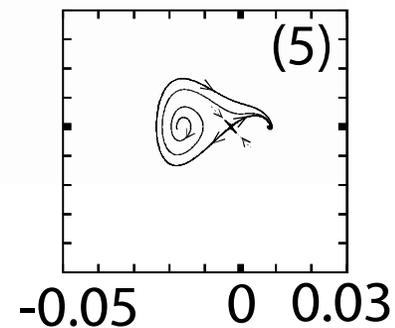
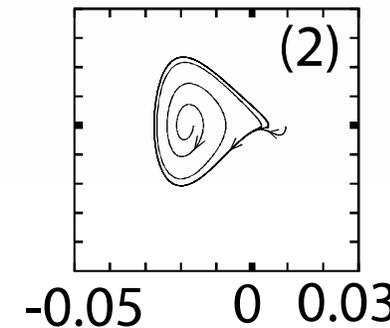
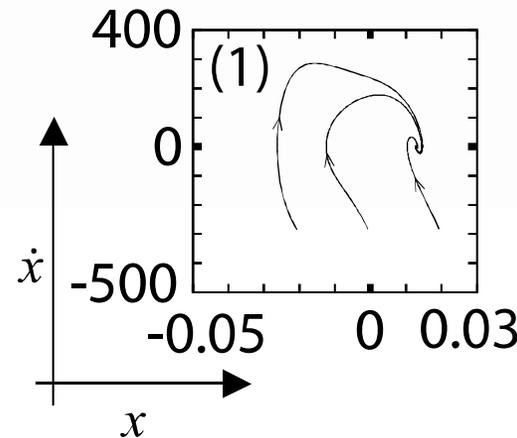
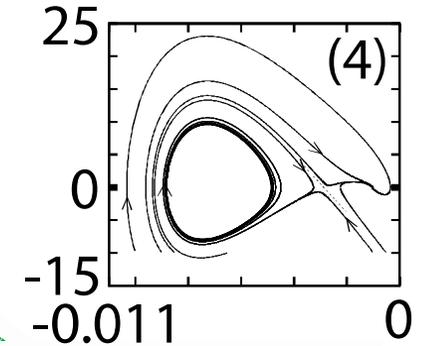
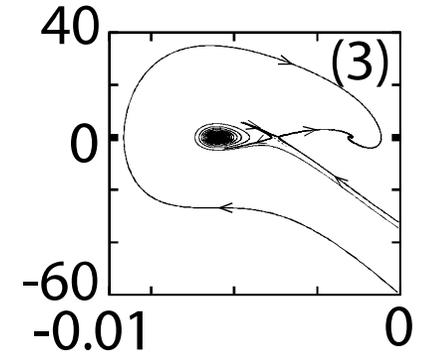
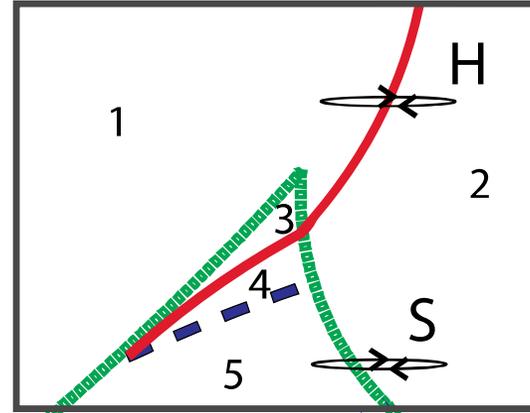
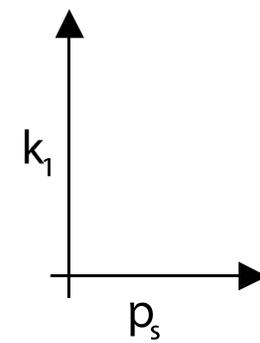
✓ frequency defined by  $k_1$

### S: SNILC:

✓ spectrally rich

✓ fundamental frequency defined by pressure

Numbers indicate regions of the parameter space with qualitative similar outputs





# Dynamical analysis of the model



Parameters  $k_1$  y  $P_s$  are related to physiological variables:

$k_1 \propto$  activity of vS syringeal muscle

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### H: Hopf:

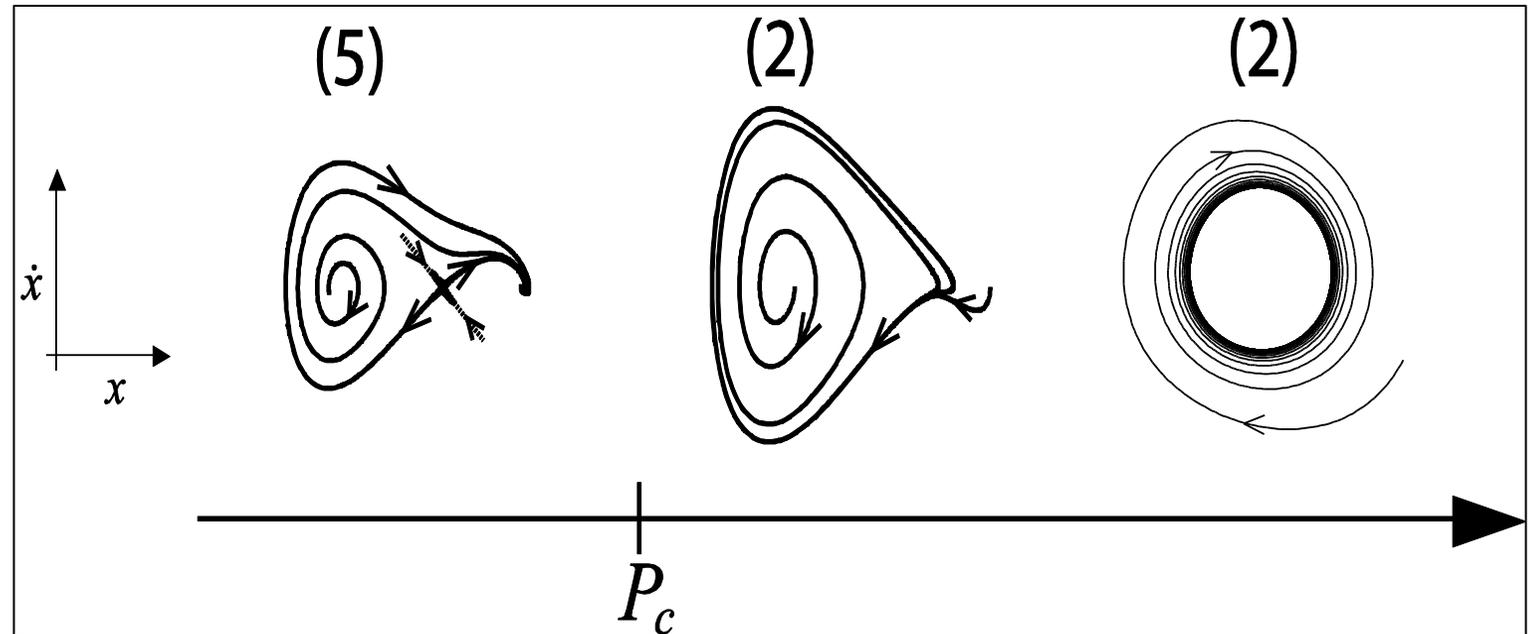
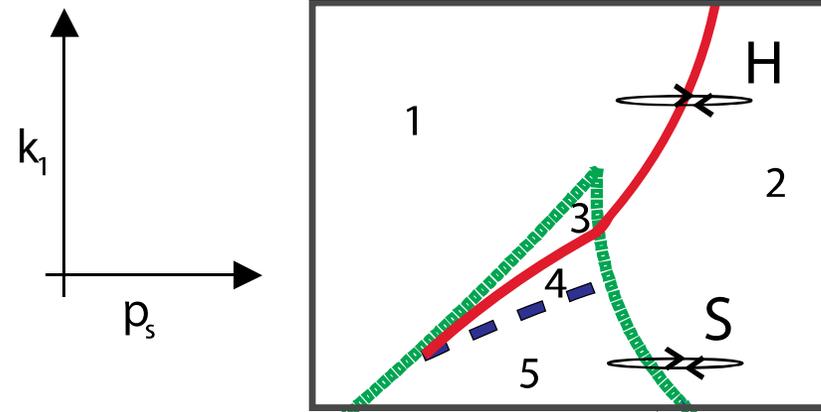
✓ almost tonal

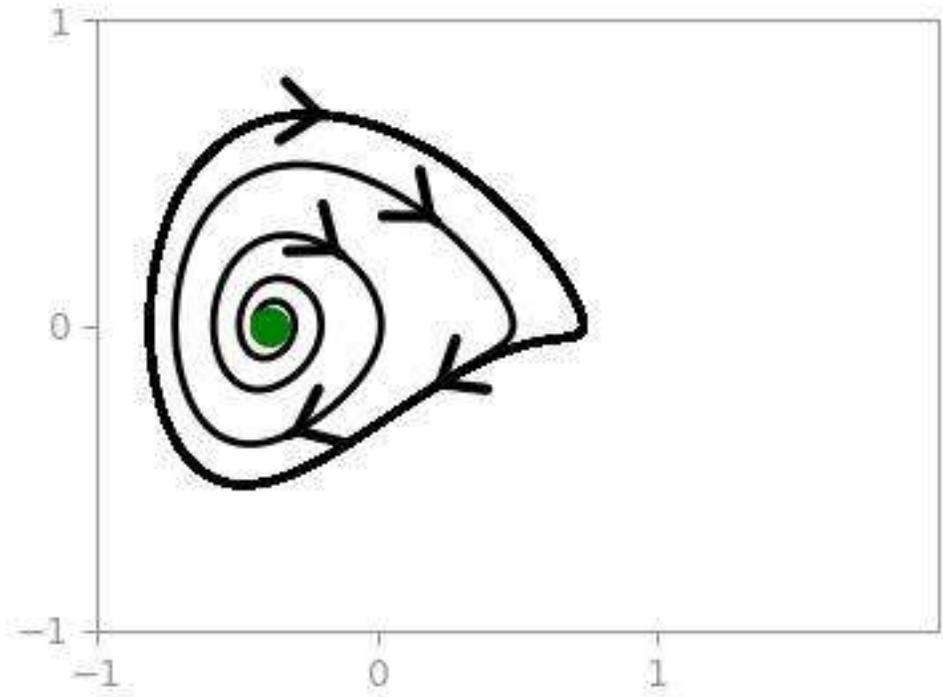
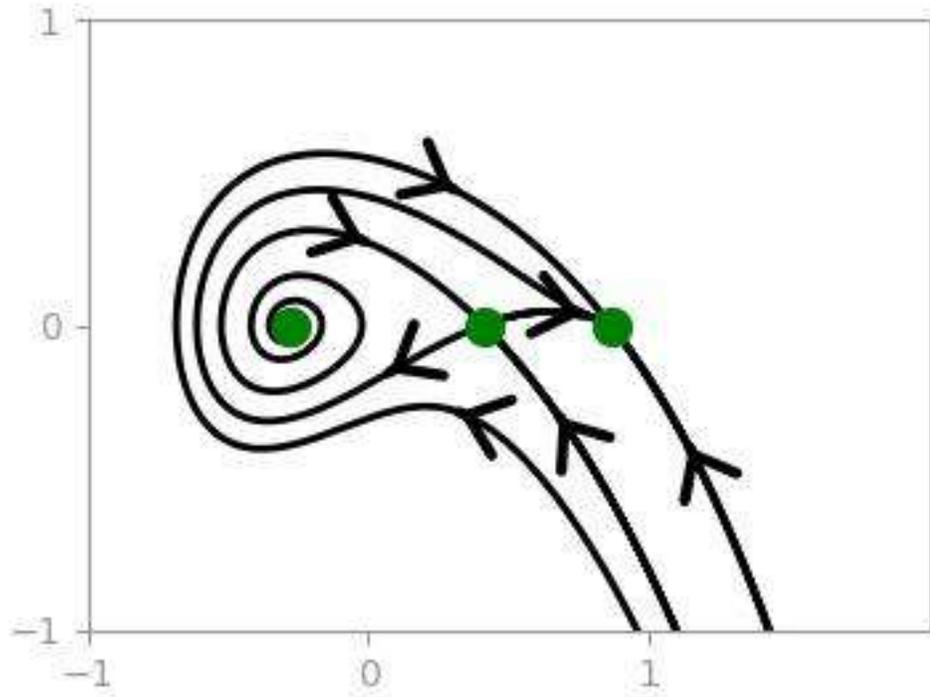
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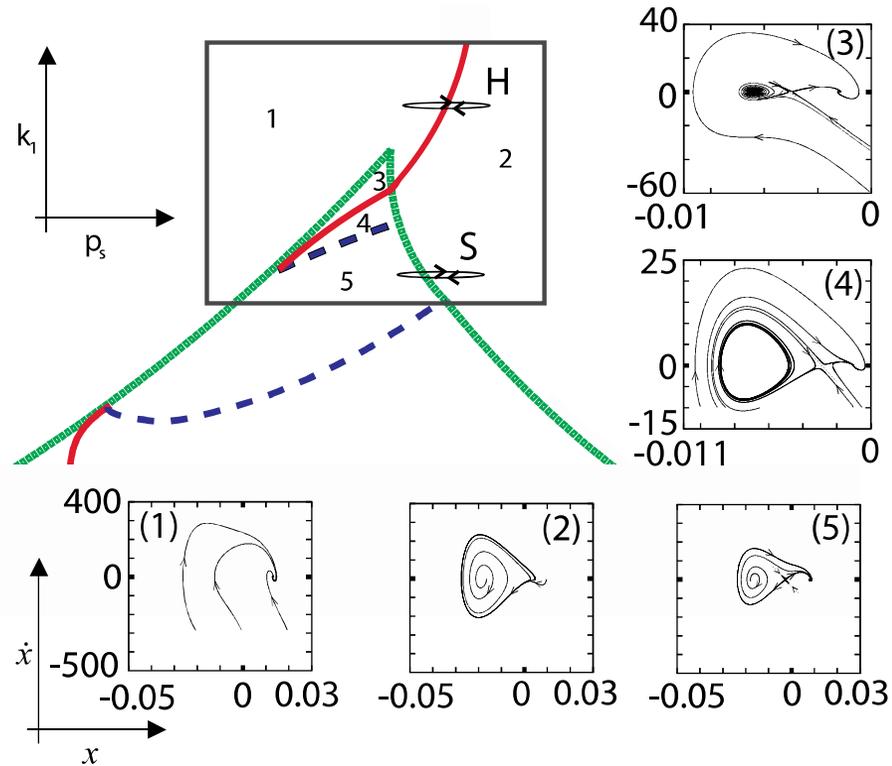




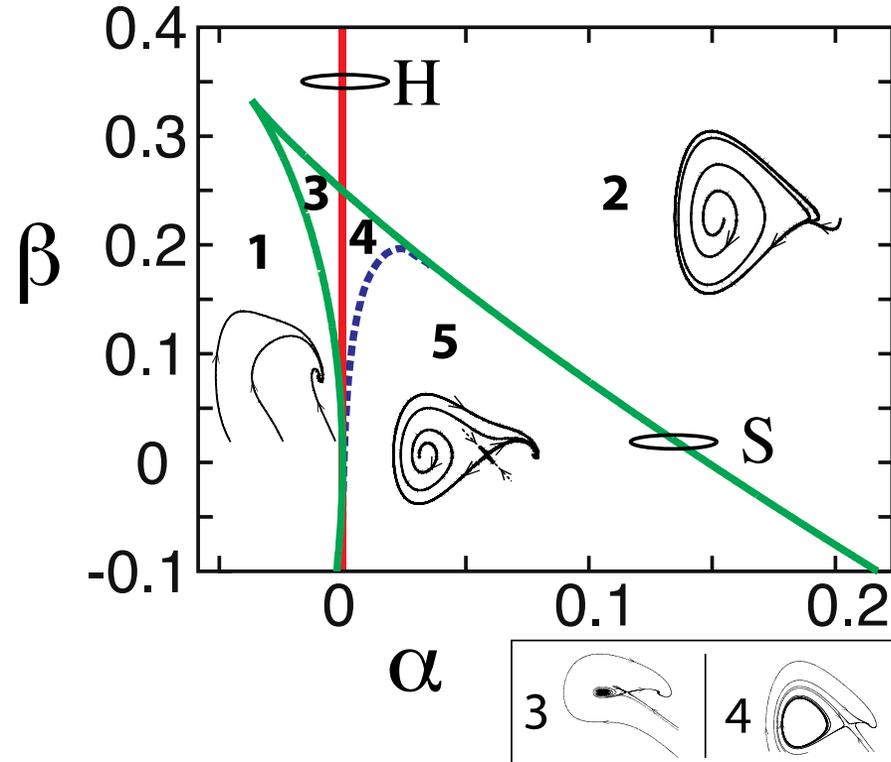
**SNILC:** one of the ways oscillations arise in 2d systems

# Normal form reduction

## Complete model



## Normal form



$$\frac{dx}{dt} = y$$

$$\frac{dy}{dt} = -\alpha(t)\gamma^2 - \beta(t)\gamma^2 x - \gamma^2 x^3 - \gamma x^2 y + \gamma^2 x^2 - \gamma x y$$



# Generating synthetic songs: source



Dynamical system model of the sound source

$$\frac{dx}{dt} = y$$

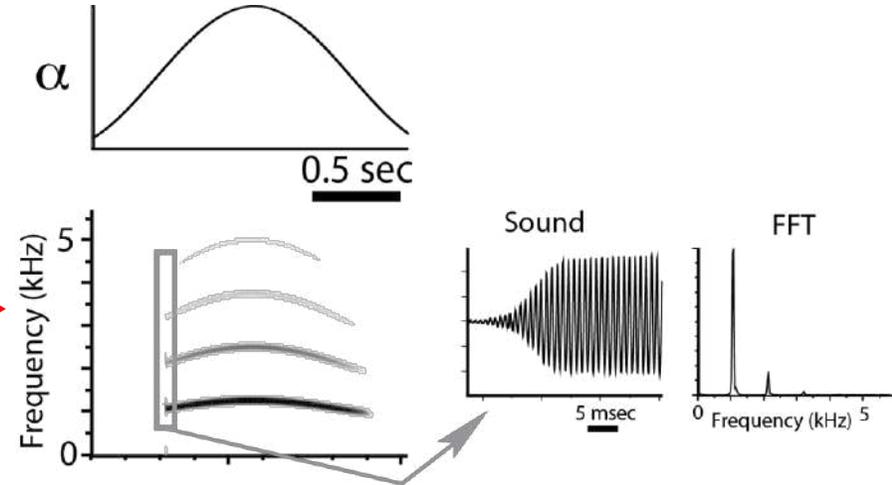
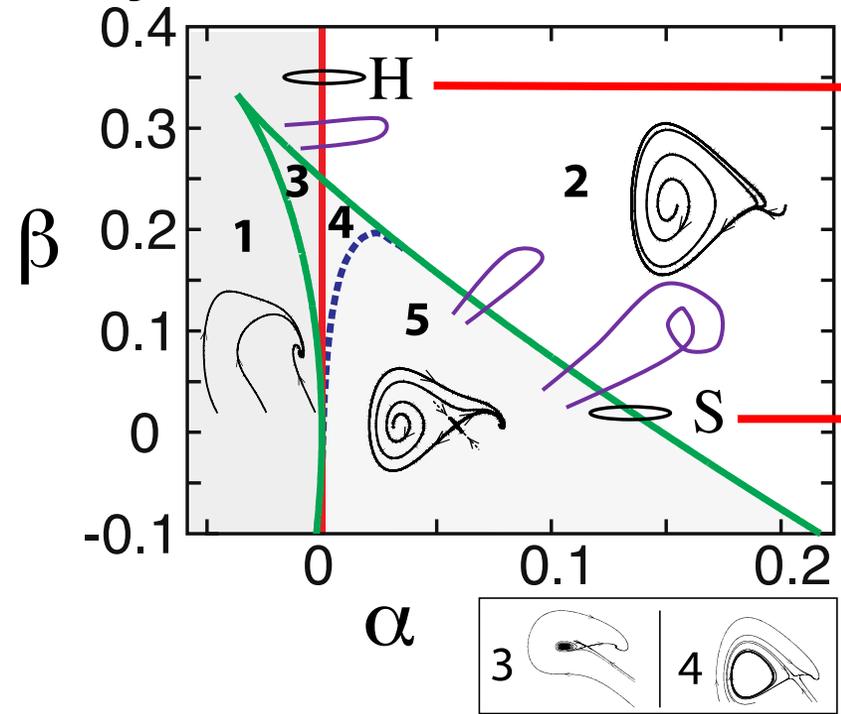
$$\frac{dy}{dt} = -\alpha(t)\gamma^2 - \beta(t)\gamma^2x - \gamma^2x^3 - \gamma x^2y + \gamma^2x^2 - \gamma xy$$

$x$ : medial position of a labium

$\alpha$ : **pressure** of the air sac system,  $\beta$ : **tension** of the syringeal labia

## Dynamical analysis of the sound source

Numbers indicate regions of the parameter space with qualitative similar outputs





# Generating synthetic zebra finch songs

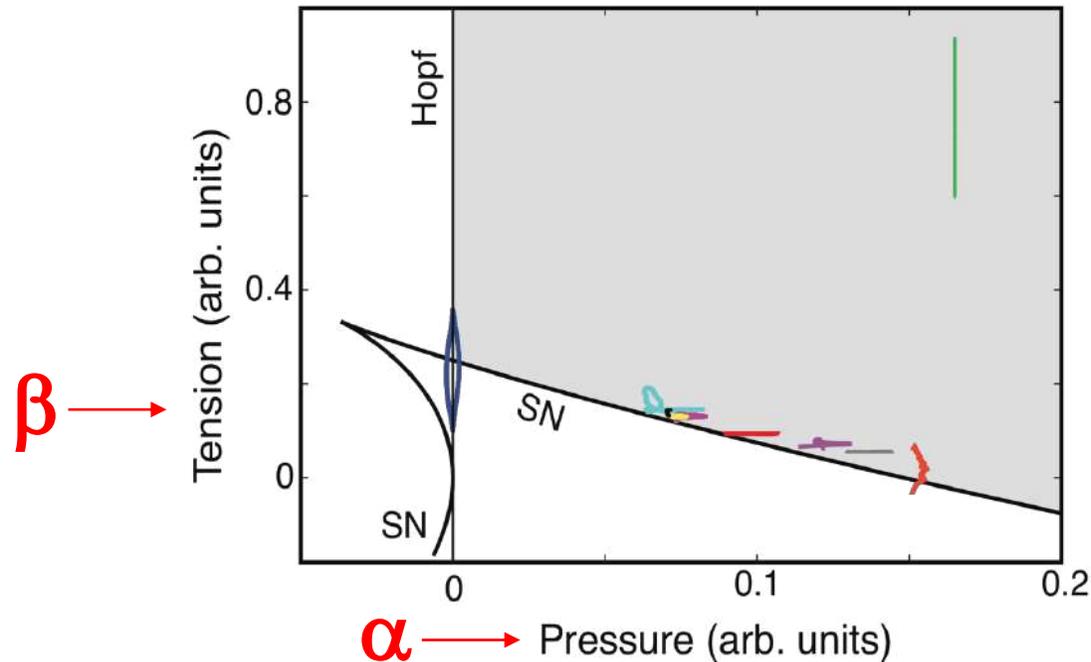
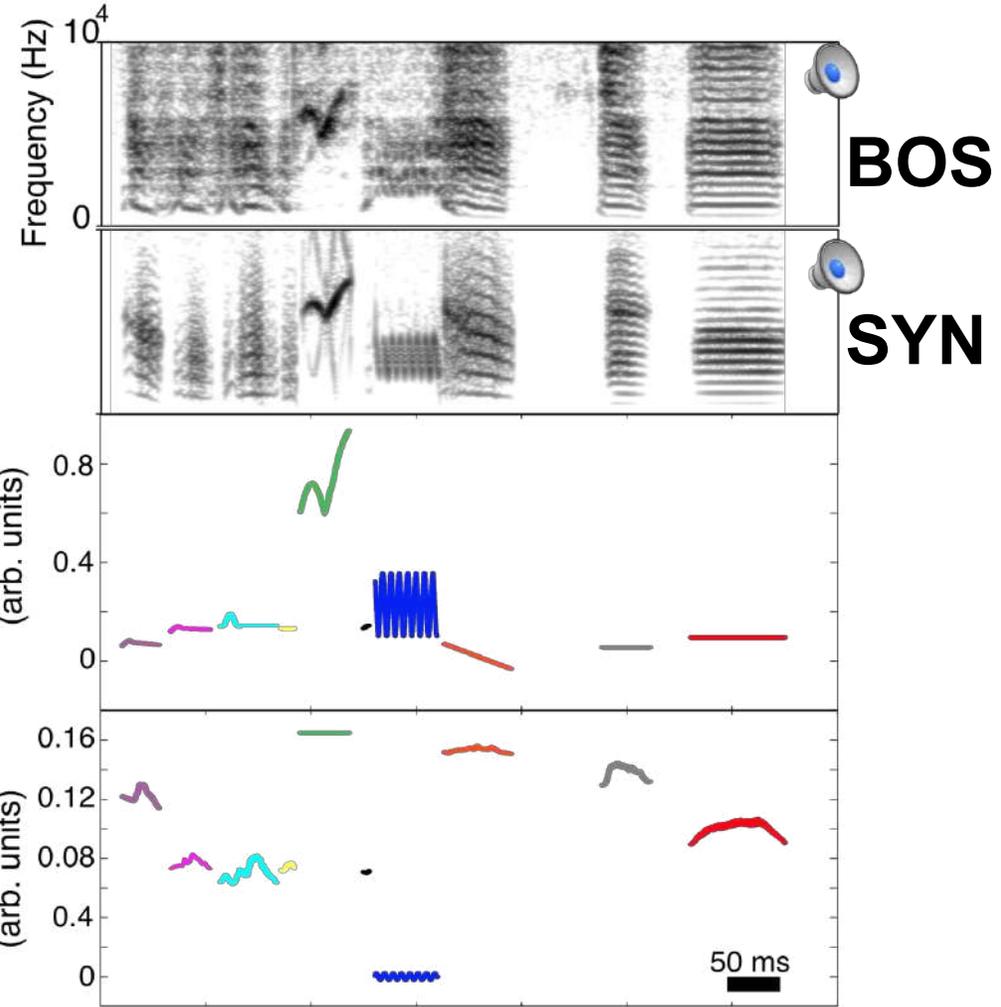


$$\frac{dx}{dt} = y$$

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$x$ : medial position of a labium  
 $\alpha$ : **pressure** of the air sac system  
 $\beta$ : **tension** of the syringeal labia  
 $\gamma$ : scale factor

Looks good!  
 Sounds good!  
 But is this relevant?





# Synthetic copies of zebra finch song

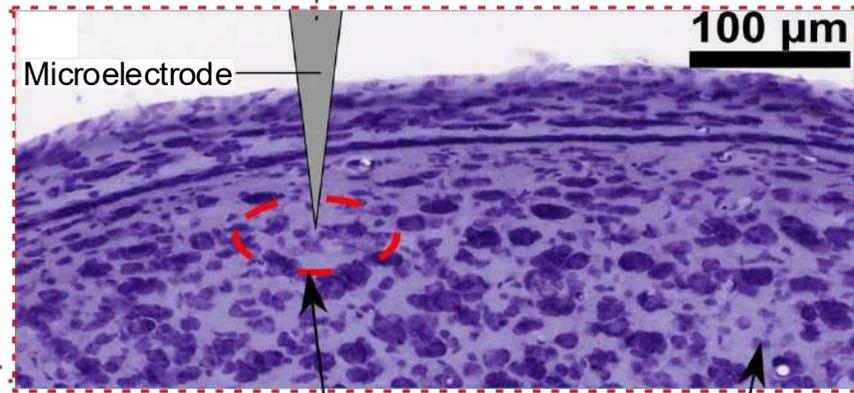
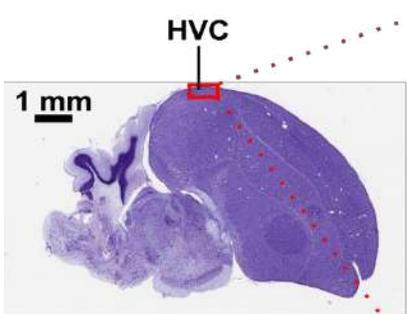
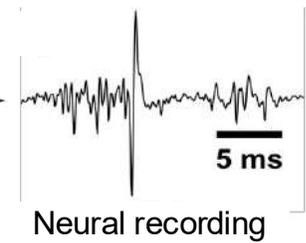


Neural recordings to validate the model

Ask the bird!



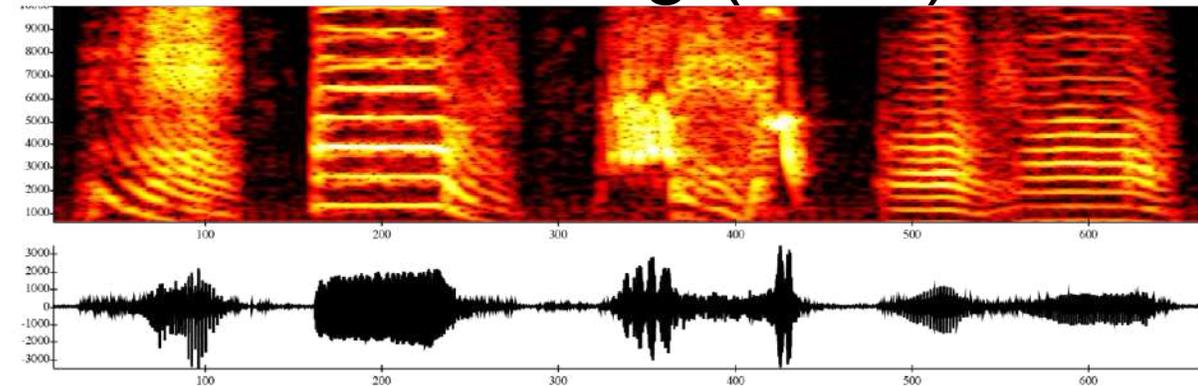
Extracellular recordings



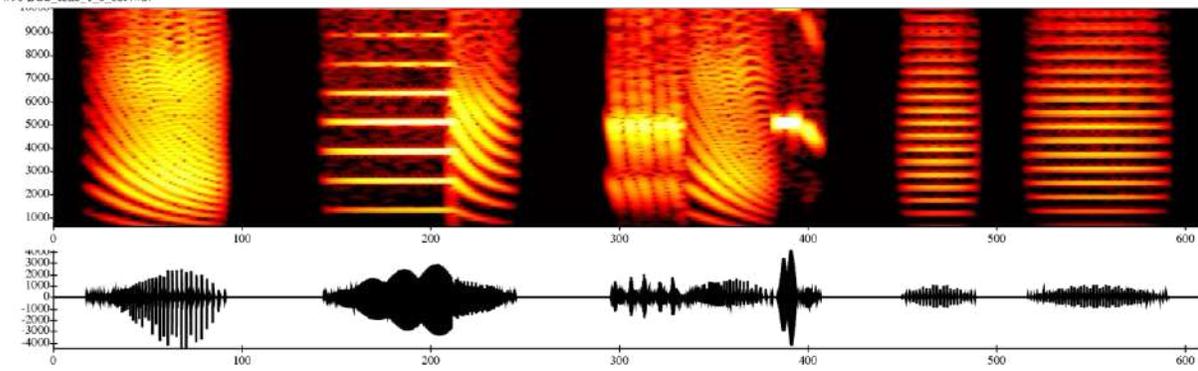
Detection radius

Neuronal soma

Bird's Own Song (BOS)



w96-BOS\_sono\_1\_0\_689.wav



w96-SYNHok\_sono\_1\_0\_608.wav

Synthetic copy (SYN)



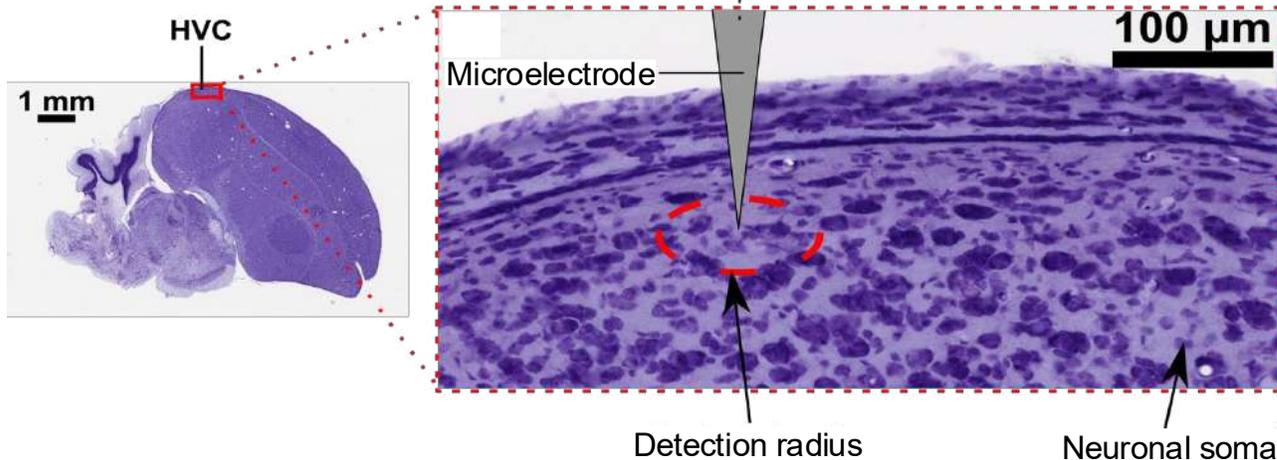
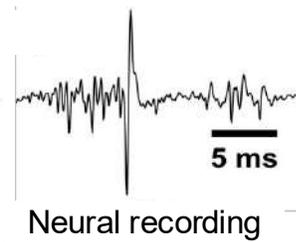
# Testing the model



Neural recordings to validate the model



Extracellular recordings



Neural selectivity in the song system

Neurons respond to the bird's own song (BOS) with a distinctive pattern.

# Testing the model



Selective neurons to the bird's own song (BOS)



Neurons code for  
the bird's own  
song (BOS)  
when singing

# Testing the model



## Selective neurons to the bird's own song (BOS)



The auditory presentation during sleep elicits the same pattern of response than during singing.

The response is state dependent (nothing if the bird wakes up)



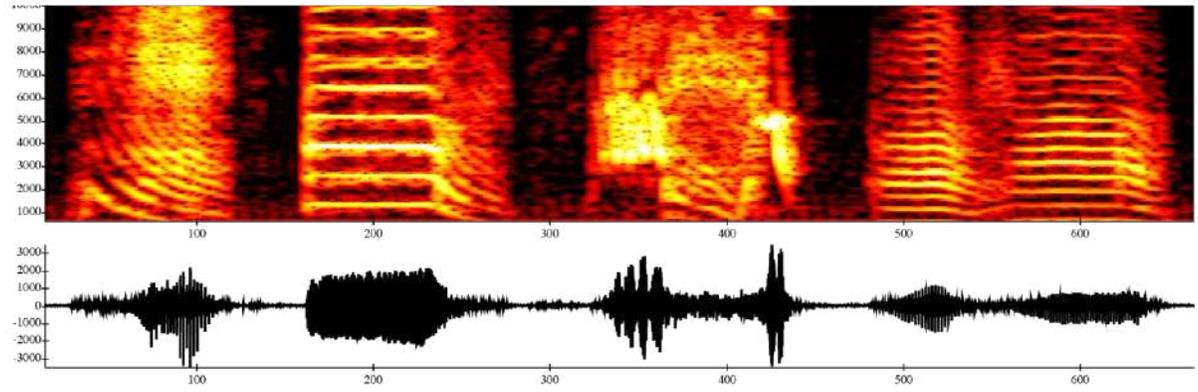
# Synthetic copies of zebra finch song



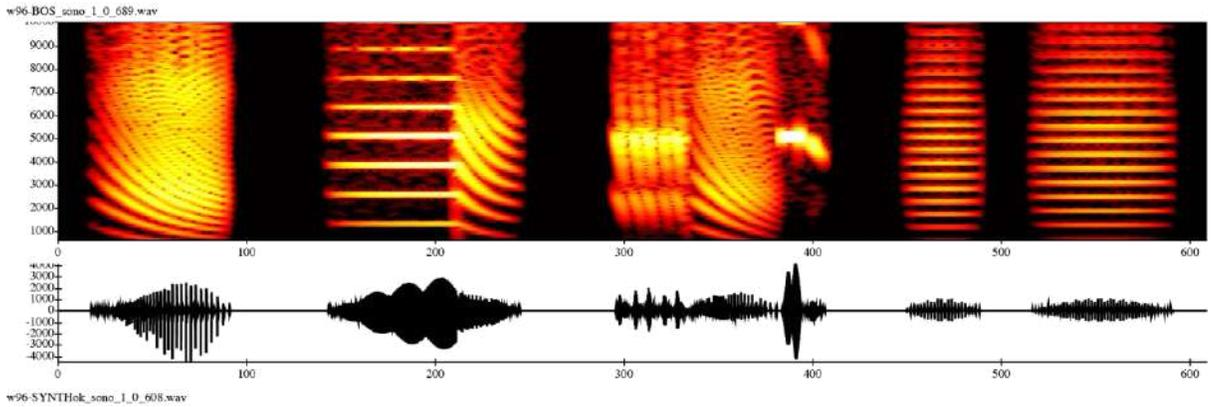
$$\frac{dx}{dt} = y$$
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$x$ : medial position of a labium  
 $\alpha$ : pressure of the air sac system  
 $\beta$ : tension of the syringeal labia  
 $\gamma$ : scale factor

Zebra finch song



BOS 

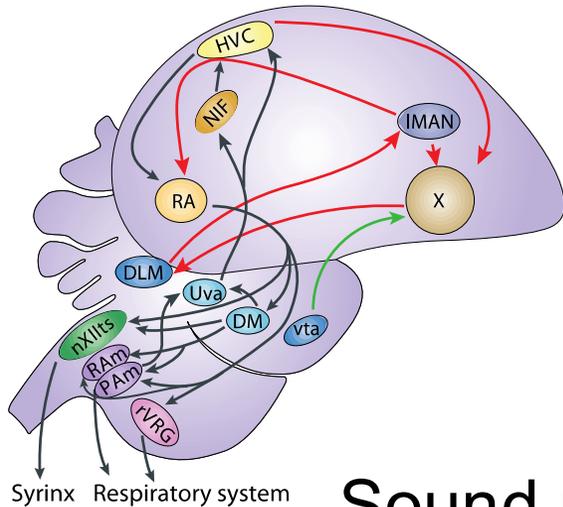
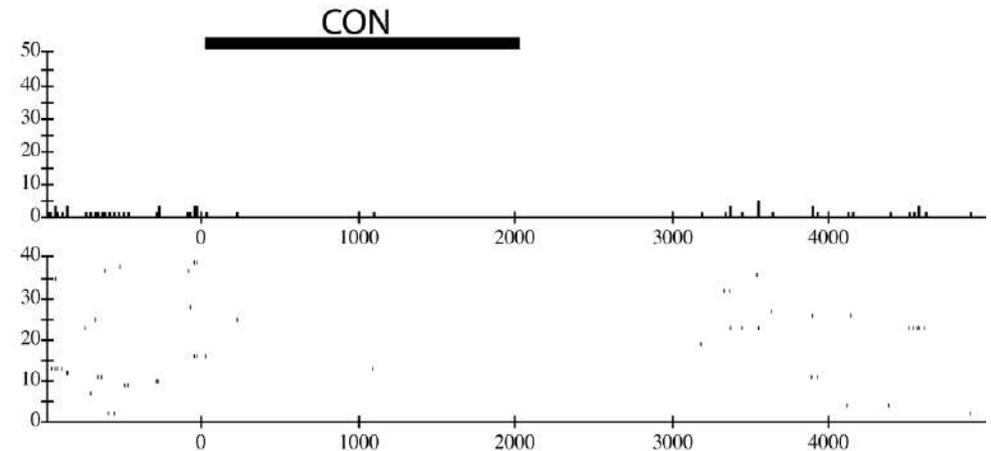
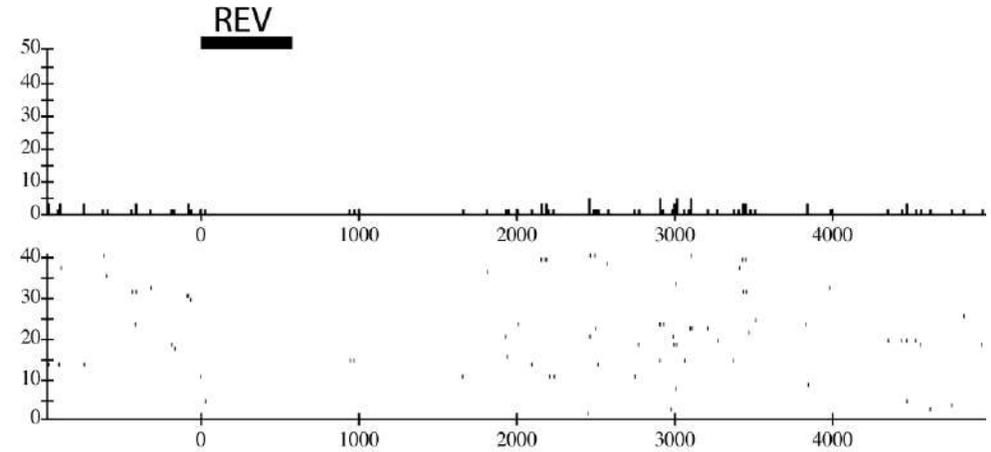
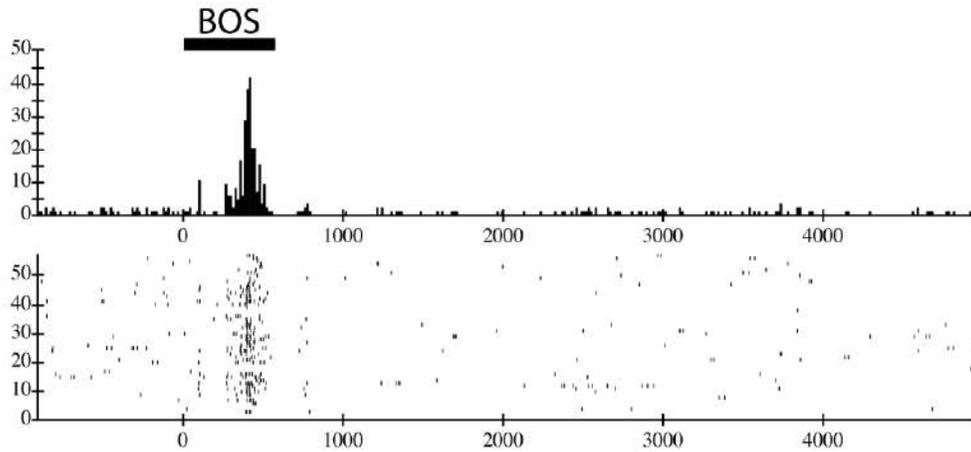


SYN 

# Testing the model

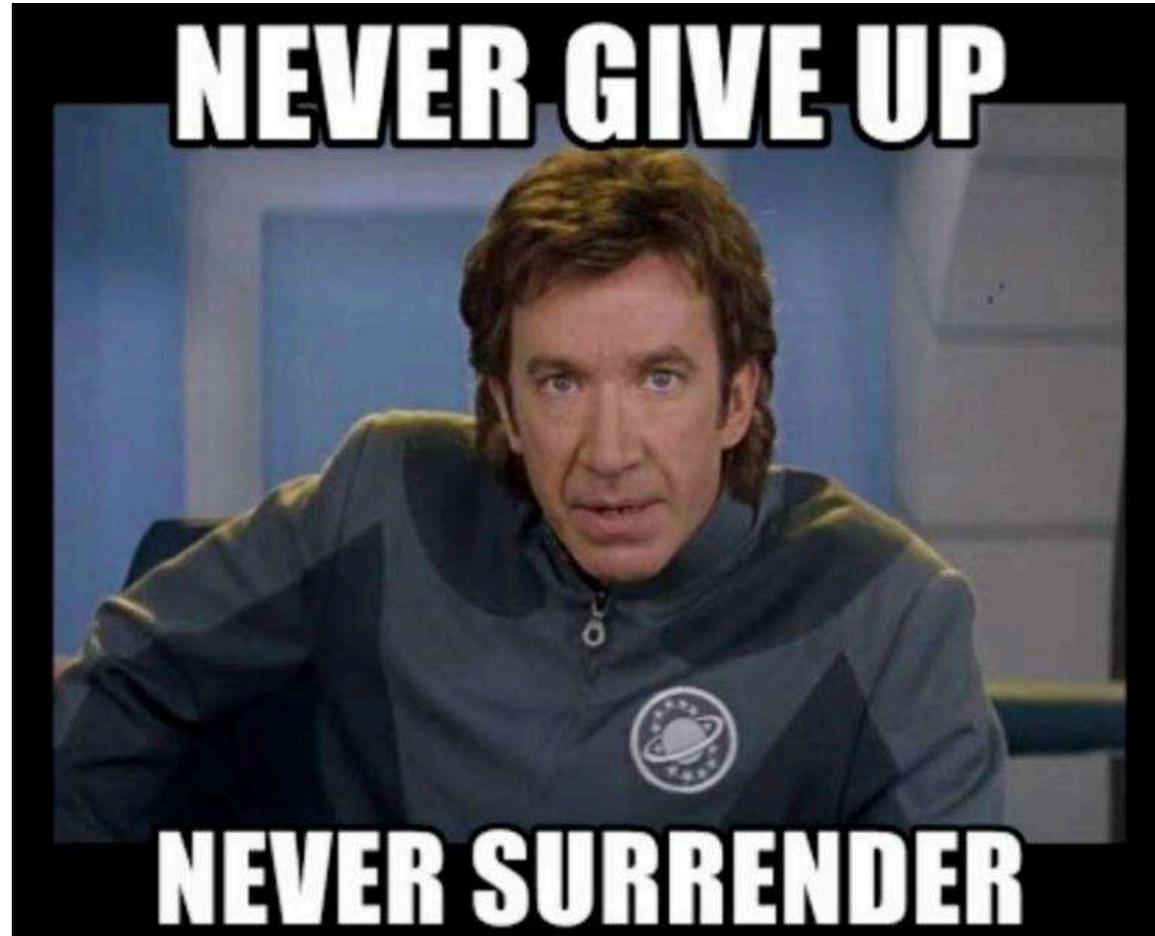


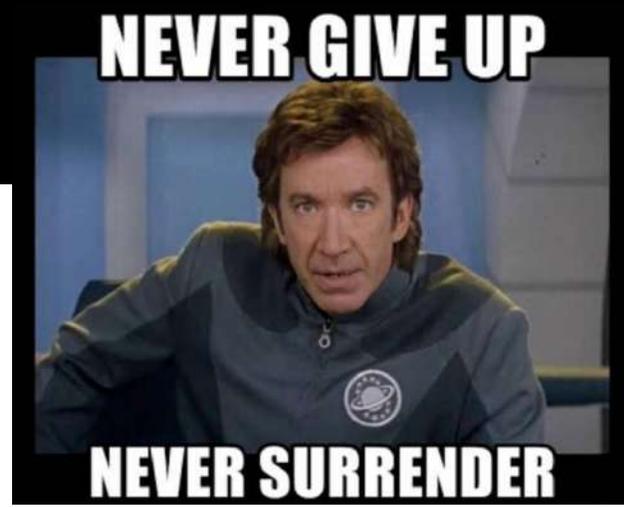
Neurons in HVC respond selectively to the Bird's Own Song (BOS)



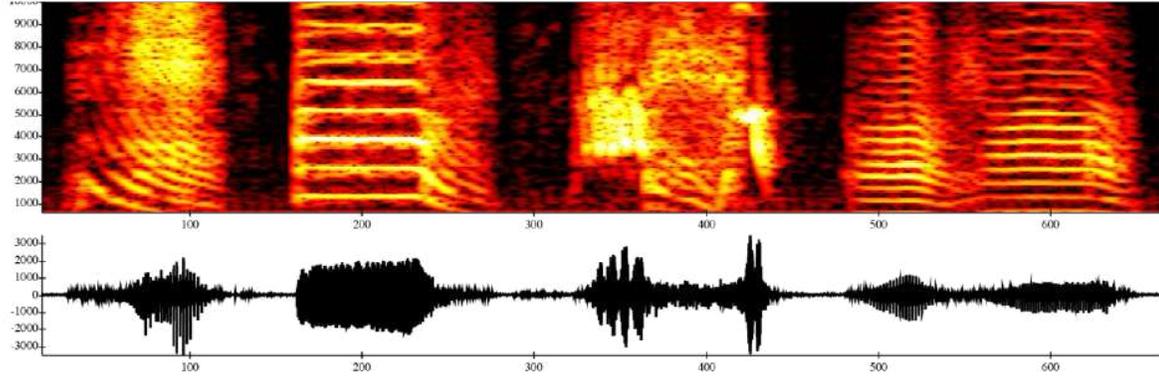
Sound presentation during sleep

What do we do now ???



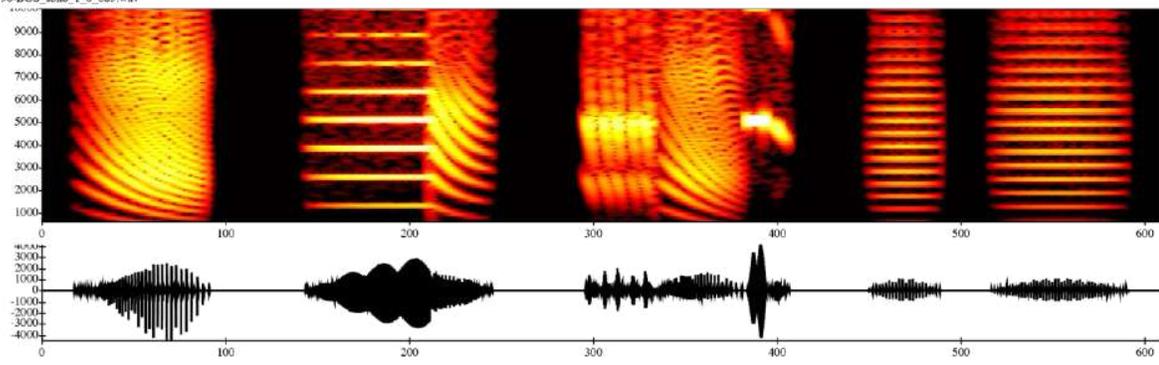


BOS



w96-BOS\_sono\_1\_0\_689.wav

SYN



w96-SYNHok\_sono\_1\_0\_608.wav

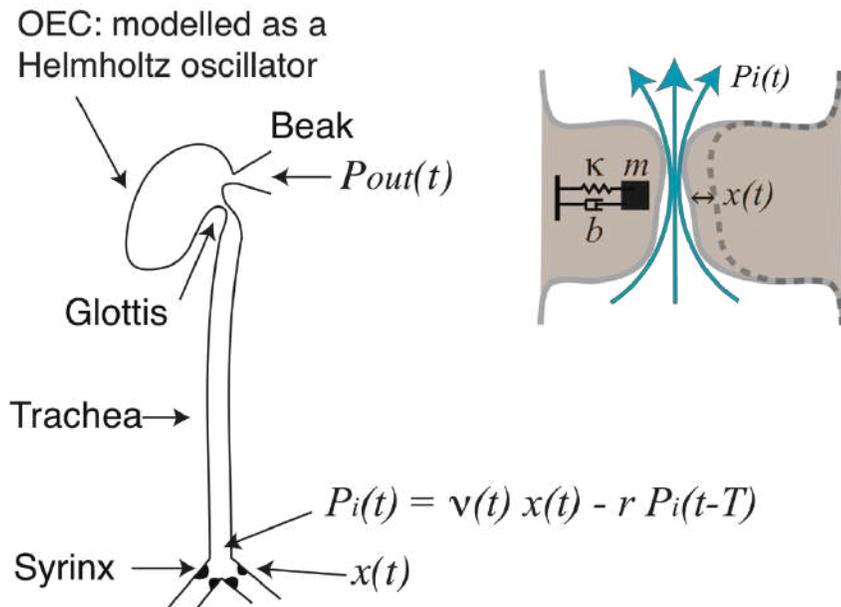
The challenge is to remain simple!

This is not working

# A more detailed modeling



- ✓ More detailed modeling of the vocal tract (before: 3 tubes).
- Oropharyngeal cavity as a resonator**
- ✓ **Noise** in the labial tension (controlled by syringeal muscles)

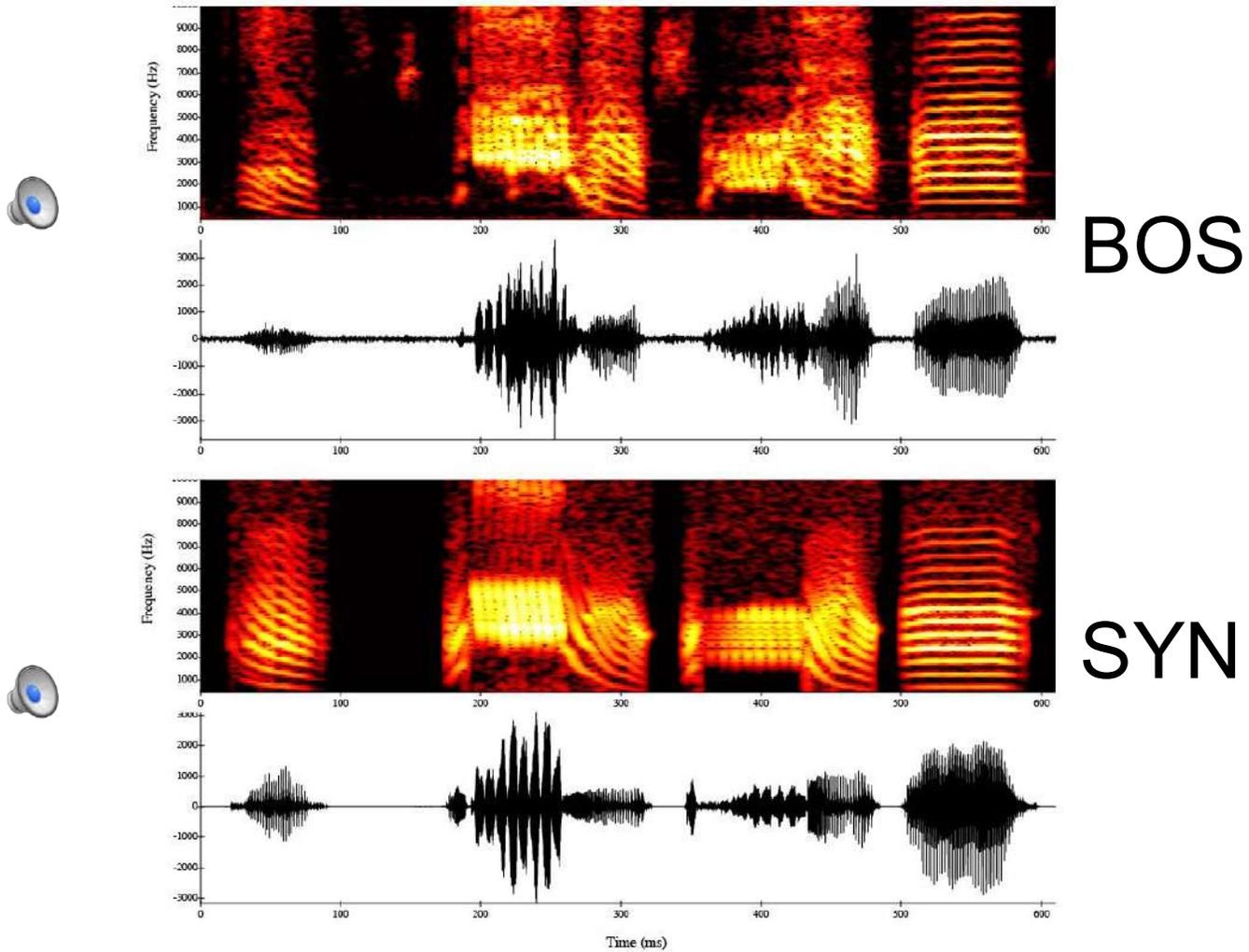


$$\frac{dx}{dt} = y$$

$$\frac{dy}{dt} = -\alpha(t)\gamma^2 - \beta(t)\gamma^2 x - \gamma^2 x^3 - \gamma x^2 y + \gamma^2 x^2 - \gamma x y$$

Same source

# A more detailed modeling

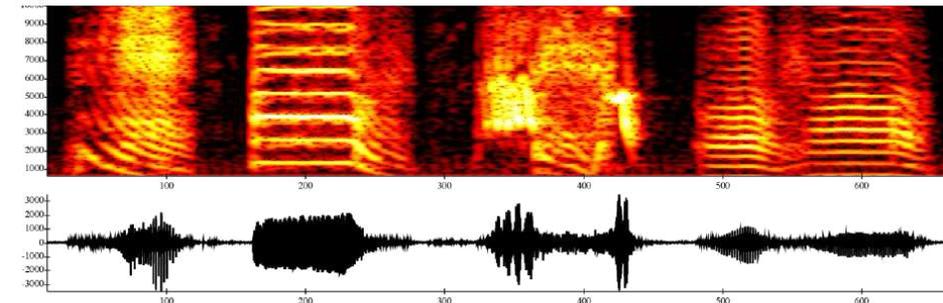


# A more detailed modeling

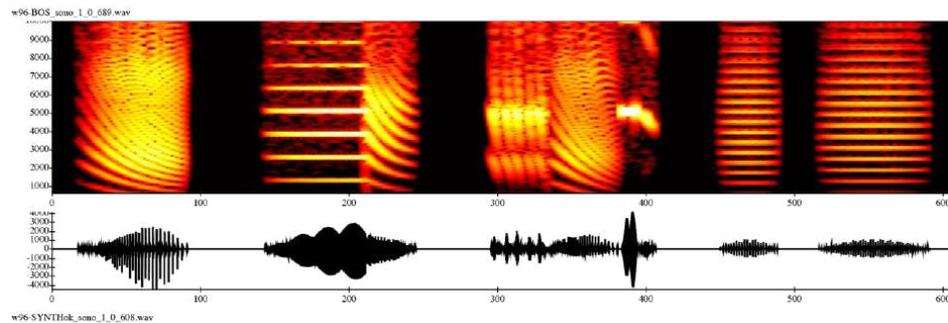


## Before

BOS



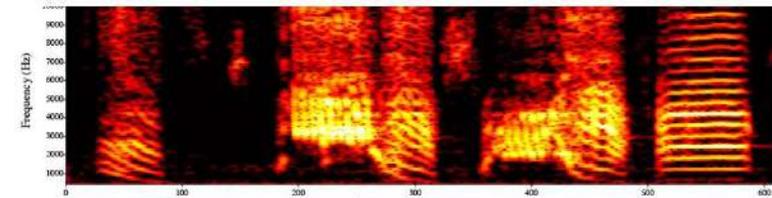
SYN



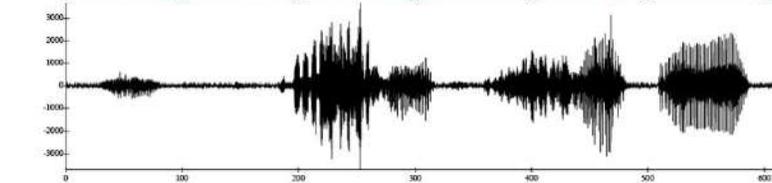
- No noise in Vs activity
- No oropharyngeal cavity

## After

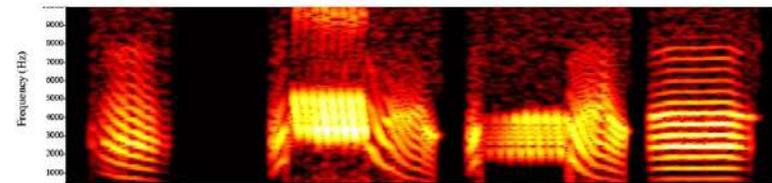
BOS



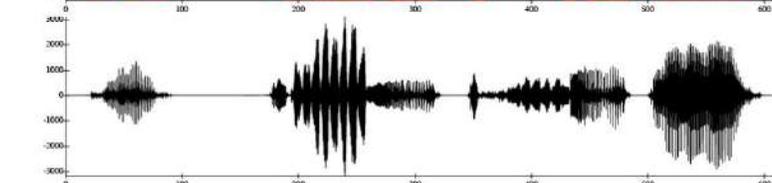
BOS



SYN



SYNTH



- ✓ Noise in Vs activity
- ✓ Oropharyngeal cavity

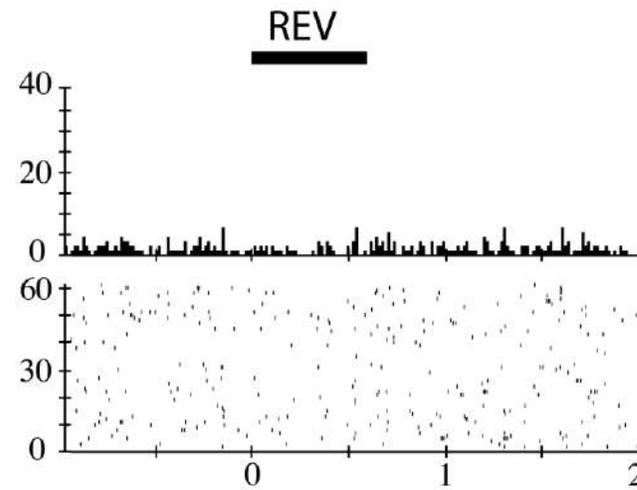
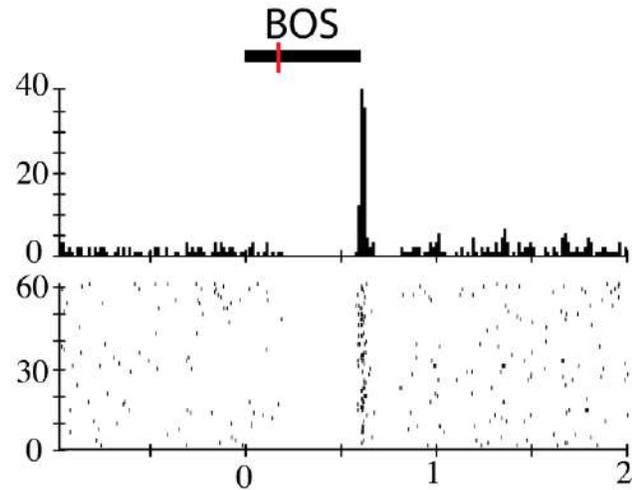
# Synthetic copies of zebra finch song



## Neural selectivity in the song system



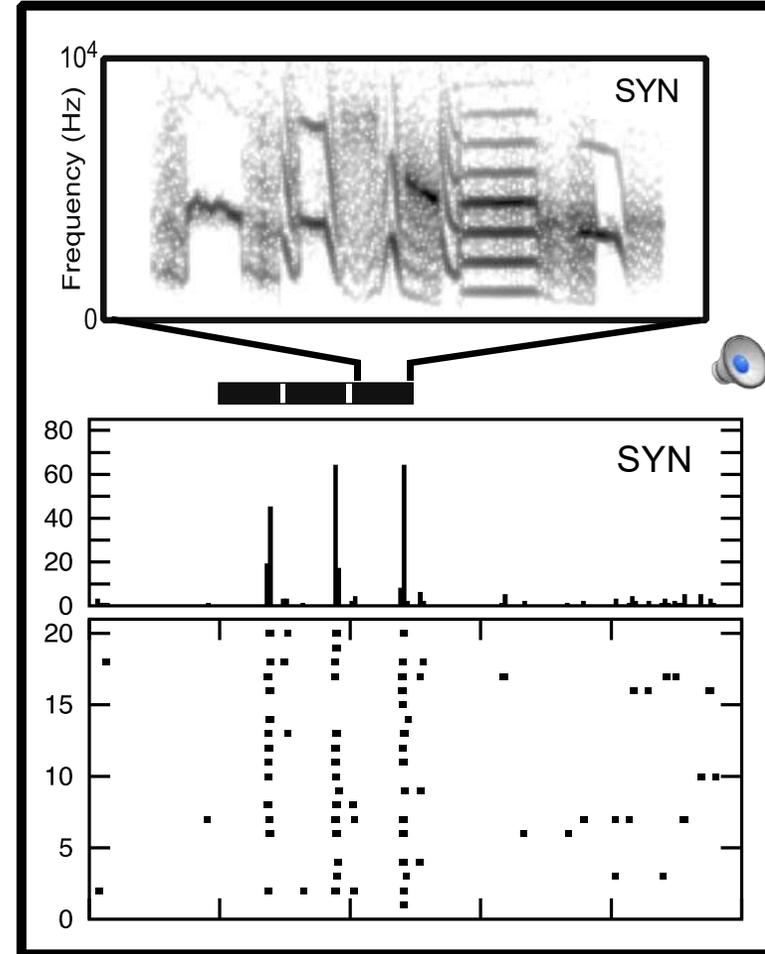
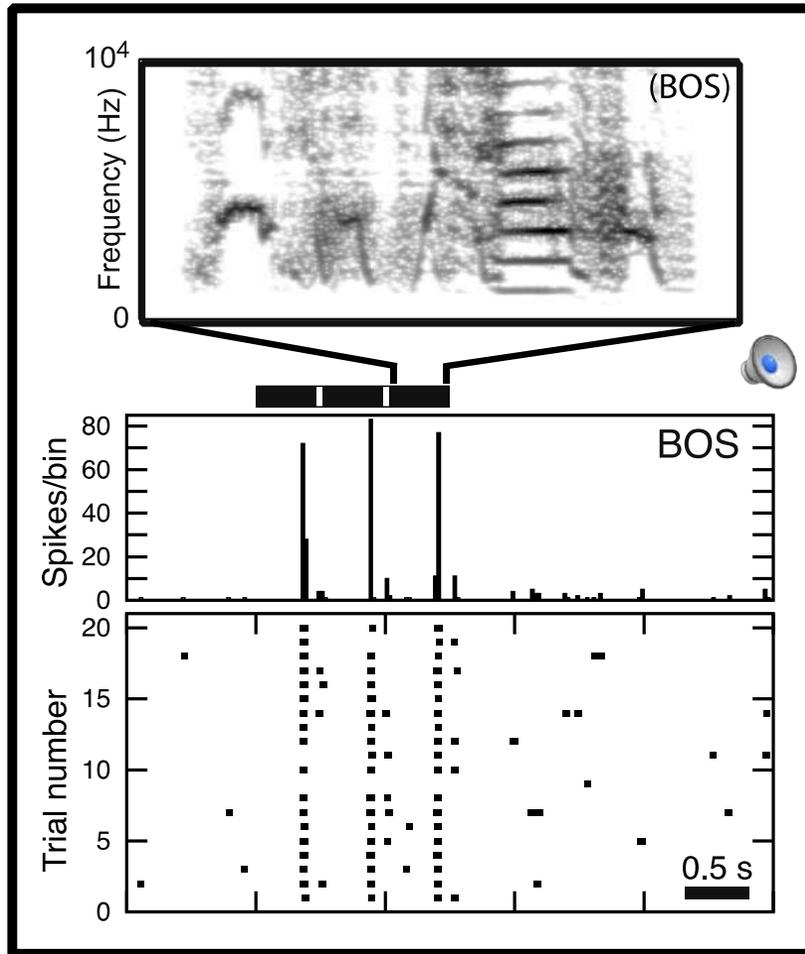
Extracellular recordings in HVC (sensorimotor nucleus)



The synthetic song elicits the same neural response than the bird's own song



# A more detailed modeling

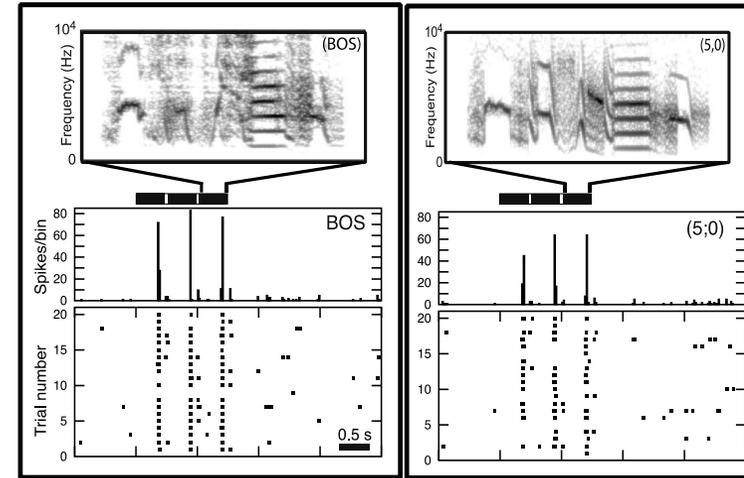


The synthetic song elicits the same neural response than the bird's own song

# Partial summary

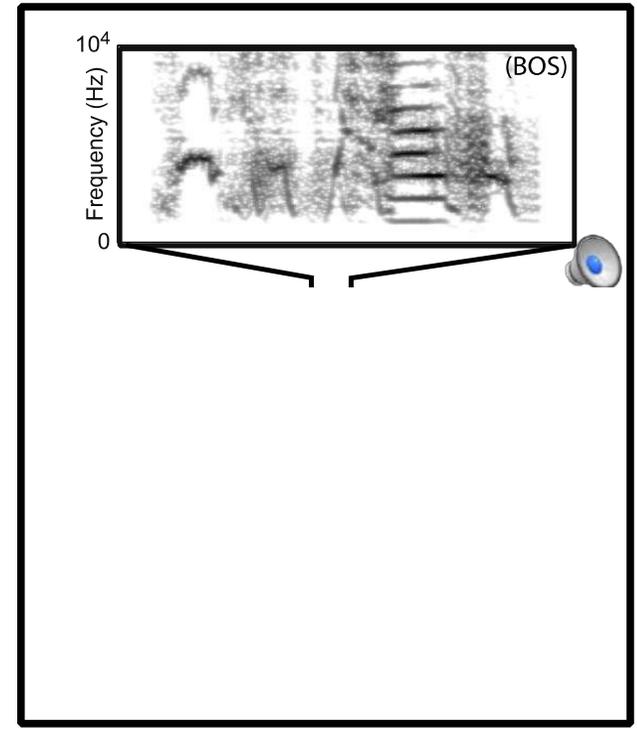
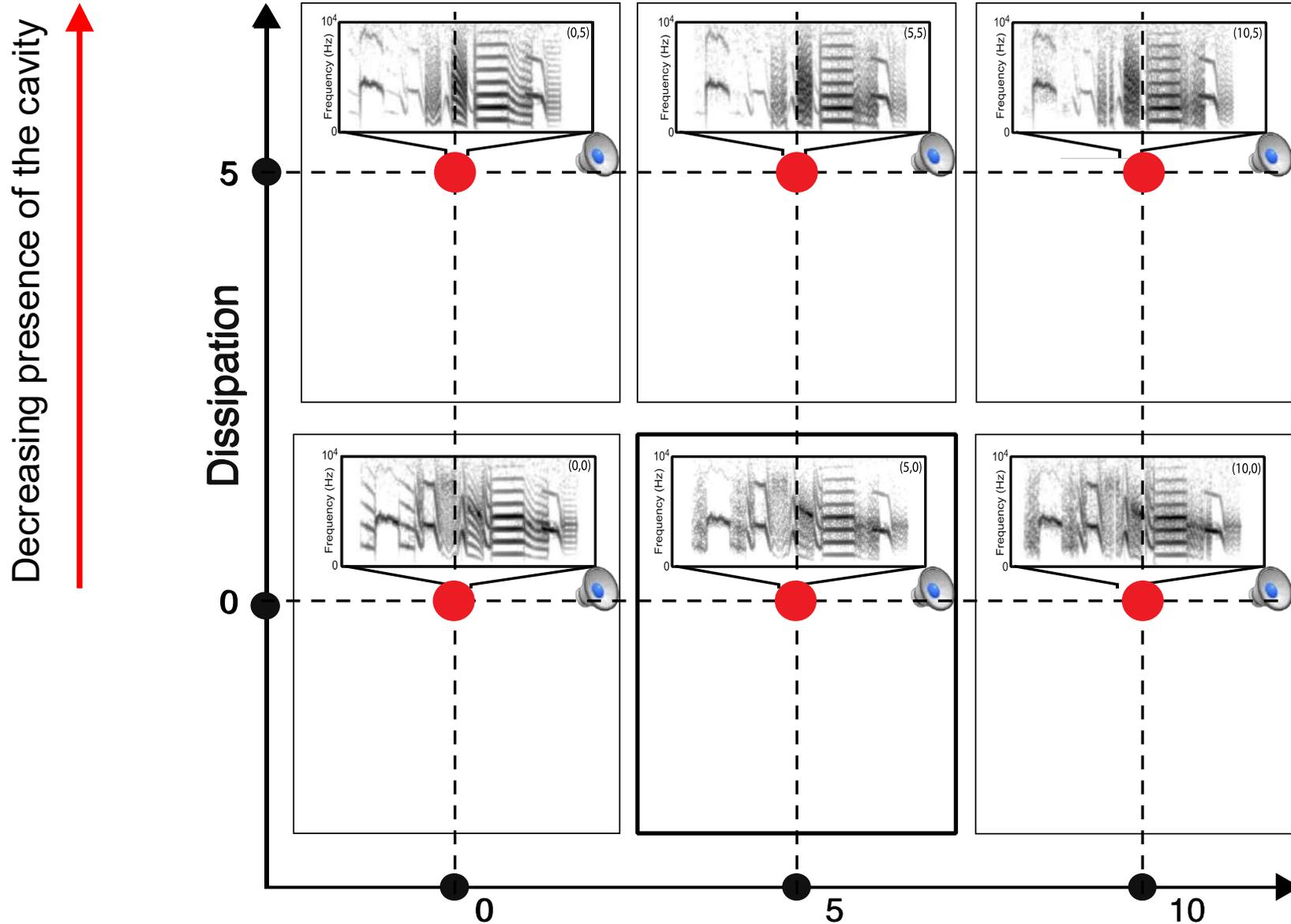


- A **minimal model** is able to generate **complex behavior** that is coded by neurons in the same way as natural behavior.



- We can now use the mathematical model as a **tool** to **study motor control, auditory perception** and **neural coding in songbirds**.

# Studying relevance of static parameters



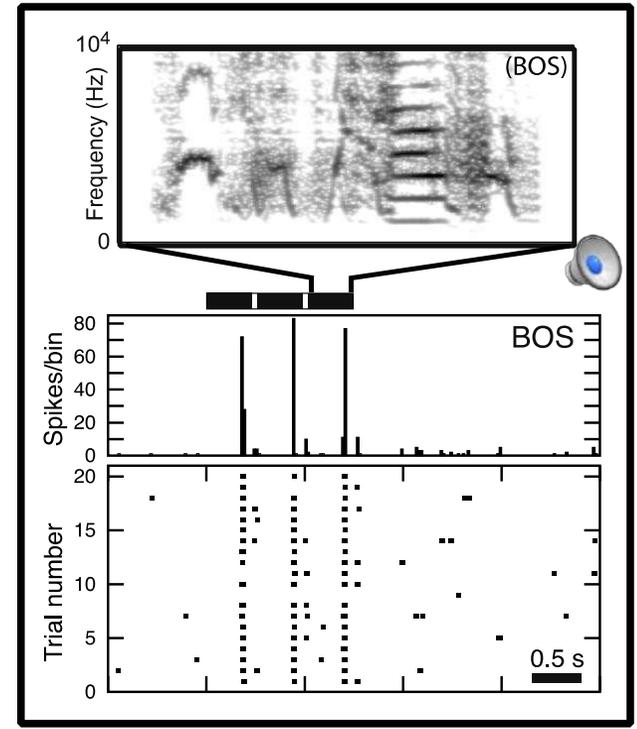
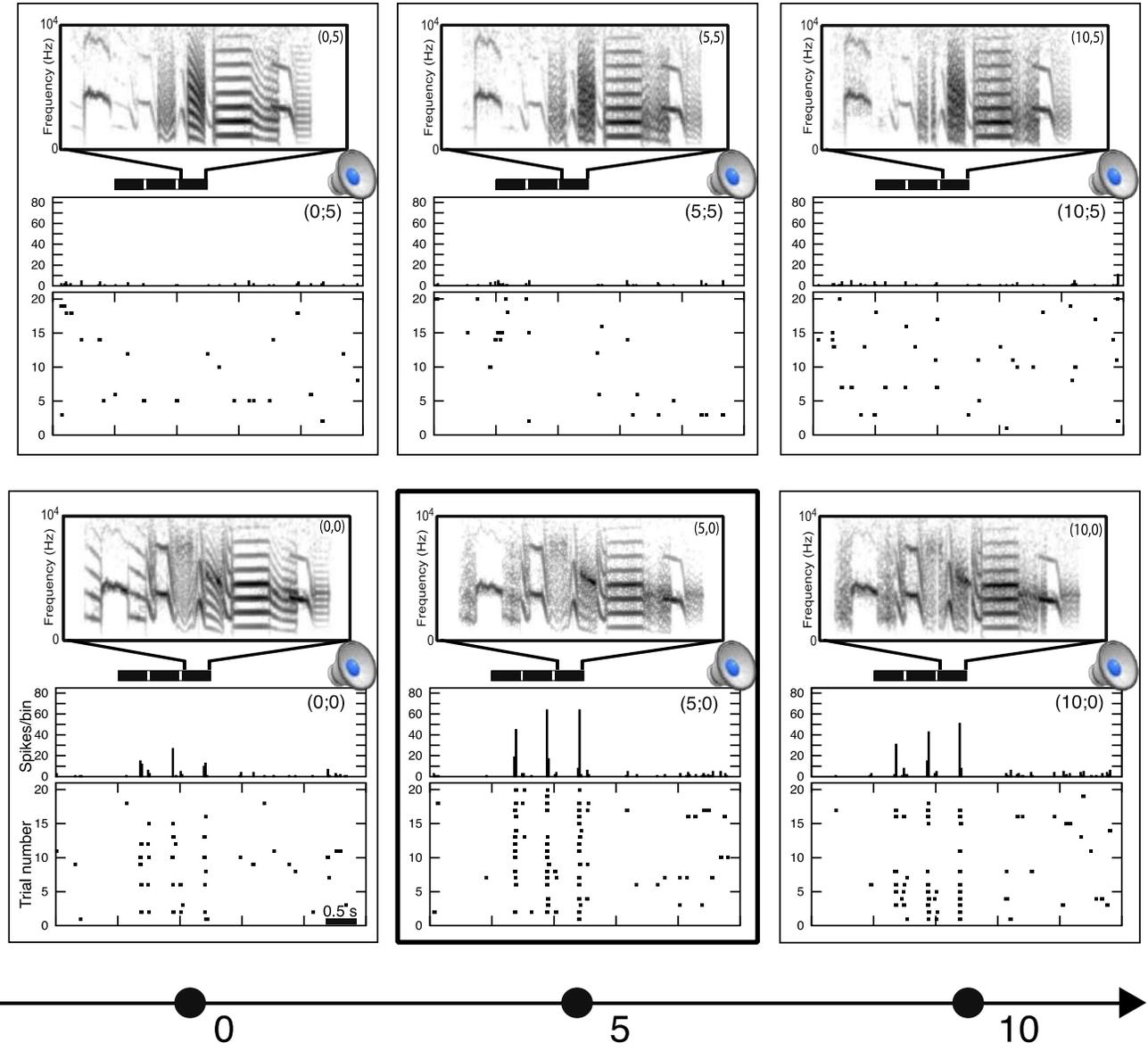
# Studying relevance of static parameters



Decreasing presence of the cavity



Dissipation





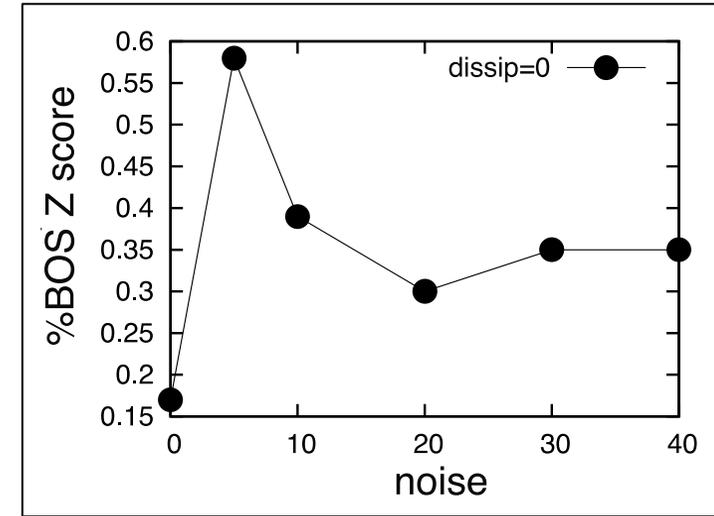
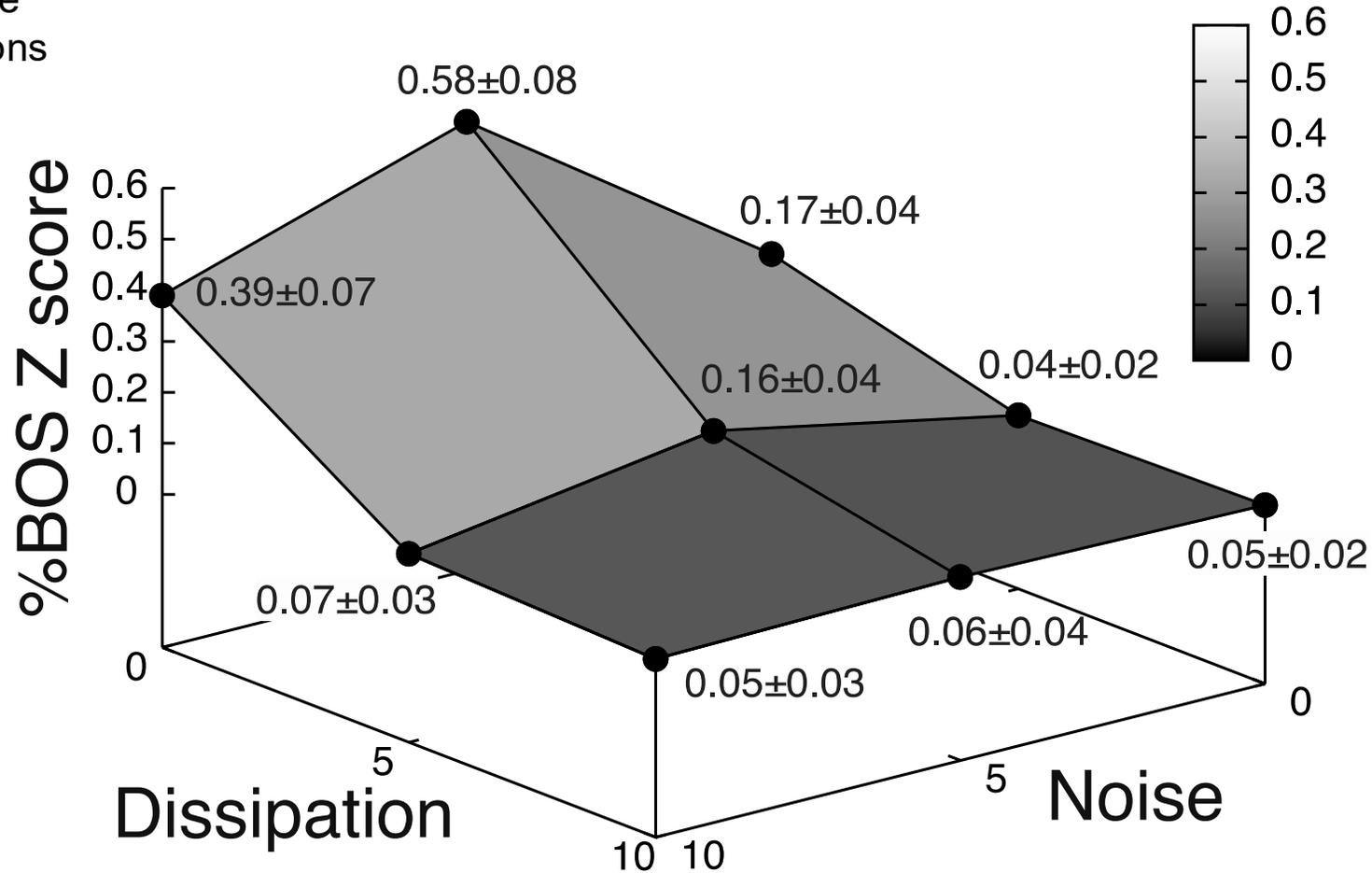
# Hierarchy of static parameter relevance



Grouped data:

- 4 birds
- 30 selective HVC neurons

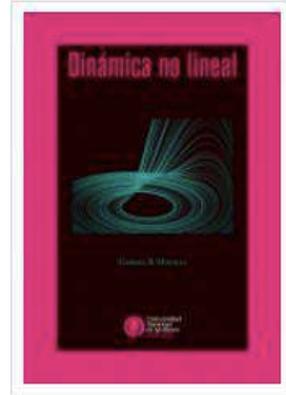
The resonant cavity is a relevant feature  
(can be controlled by the birds while singing)



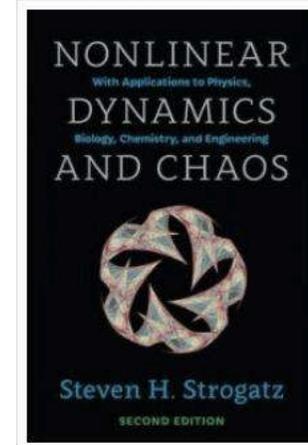
The noise has a specific value that maximizes the neural responses.

## Bibliografía **dinámica**

- Mindlin G. B. Dinámica no lineal. Editorial Universidad Nacional de Quilmes (2018)



- Strogatz, S. Nonlinear Dynamics and Chaos, Westview (fácil, muy fácil... e ideal para



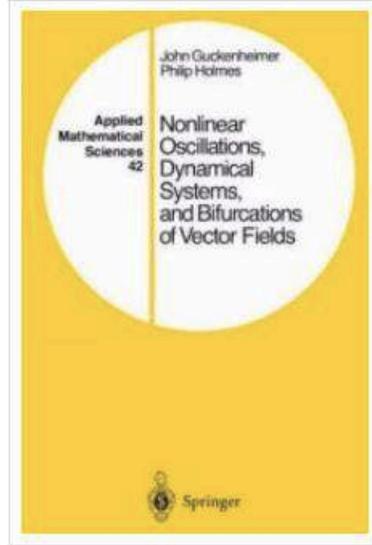
las primeras dos partes del curso)



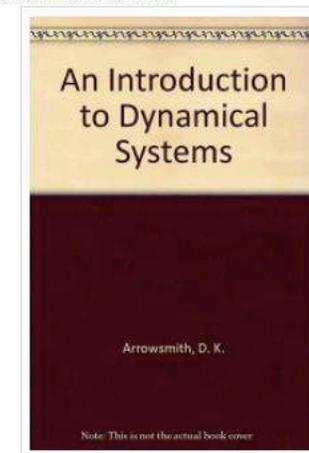
# Bibliography



- Guckenheimer J. and Holmes P. Nonlinear Oscillations, Dynamical Systems and Bifurcations of vector fields. (y... es la biblia del tema. Para el que se anime...)



- Arrowsmith D and Place C. An introduction to dynamical systems, Cambridge (duro, pero lo que se aprende aquí, sirve siempre. Ideal para la parte 3 del curso) Aperitivos para curiosos de fin de semana







Detalles técnicos para el que esté interesado





# The Hodgkin – Huxley model



Using **pioneering experimental techniques** of that time, Hodgkin and Huxley (1952) determined not only the equations but **measured all the parameters values** :

$$\begin{aligned}C \dot{V} &= I - \overbrace{\bar{g}_K n^4 (V - E_K)}^{I_K} - \overbrace{\bar{g}_{Na} m^3 h (V - E_{Na})}^{I_{Na}} - \overbrace{g_L (V - E_L)}^{I_L} \\ \dot{n} &= \alpha_n(V)(1 - n) - \beta_n(V)n \\ \dot{m} &= \alpha_m(V)(1 - m) - \beta_m(V)m \\ \dot{h} &= \alpha_h(V)(1 - h) - \beta_h(V)h ,\end{aligned}$$

Values of shifted Nernst equilibrium potentials (so that  $V_{rest} = 0$ ) :

$$E_K = -12 \text{ mV} , \quad E_{Na} = 120 \text{ mV} , \quad E_L = 10.6 \text{ mV};$$

Values of maximal conductances:

$$\bar{g}_K = 36 \text{ mS/cm}^2 , \quad \bar{g}_{Na} = 120 \text{ mS/cm}^2 , \quad g_L = 0.3 \text{ mS/cm}^2 .$$

Value of membrane capacitance:

$$C = 1 \text{ } \mu\text{F/cm}^2$$

$$\alpha_n(V) = 0.01 \frac{10 - V}{\exp\left(\frac{10 - V}{10}\right) - 1} ,$$

$$\beta_n(V) = 0.125 \exp\left(\frac{-V}{80}\right) ,$$

$$\alpha_m(V) = 0.1 \frac{25 - V}{\exp\left(\frac{25 - V}{10}\right) - 1} ,$$

$$\beta_m(V) = 4 \exp\left(\frac{-V}{18}\right) ,$$

$$\alpha_h(V) = 0.07 \exp\left(\frac{-V}{20}\right) ,$$

$$\beta_h(V) = \frac{1}{\exp\left(\frac{30 - V}{10}\right) + 1} .$$



# The Hodgkin – Huxley model



The functions  $\alpha(V)$  and  $\beta(V)$  describe the transition rates between open and closed states of the channels

The notation presented before was used only for historical reasons.

It is more convenient to use:

$$\dot{n} = (n_{\infty}(V) - n) / \tau_n(V),$$

$$\dot{m} = (m_{\infty}(V) - m) / \tau_m(V),$$

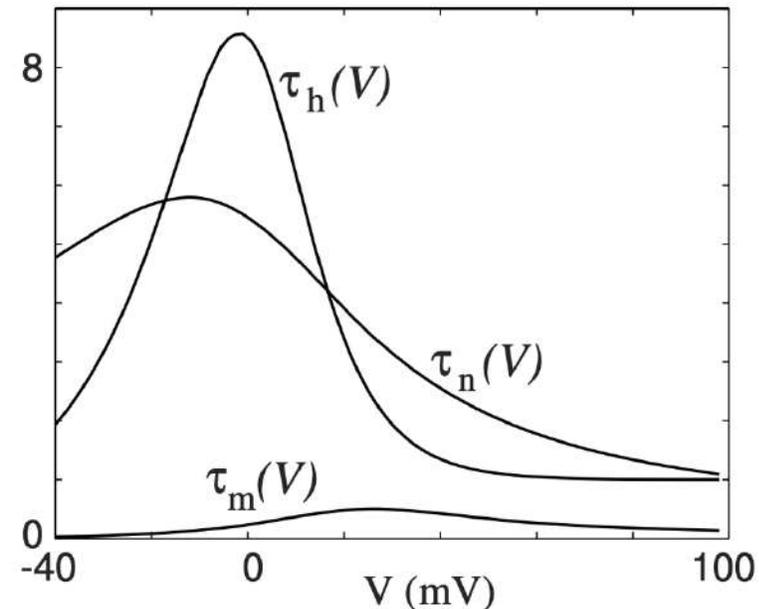
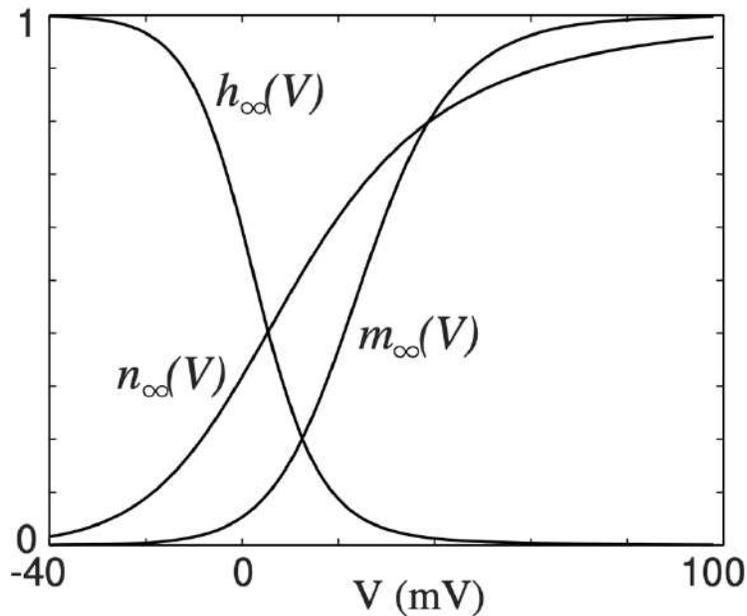
$$\dot{h} = (h_{\infty}(V) - h) / \tau_h(V),$$

where

$$n_{\infty} = \alpha_n / (\alpha_n + \beta_n), \quad \tau_n = 1 / (\alpha_n + \beta_n),$$

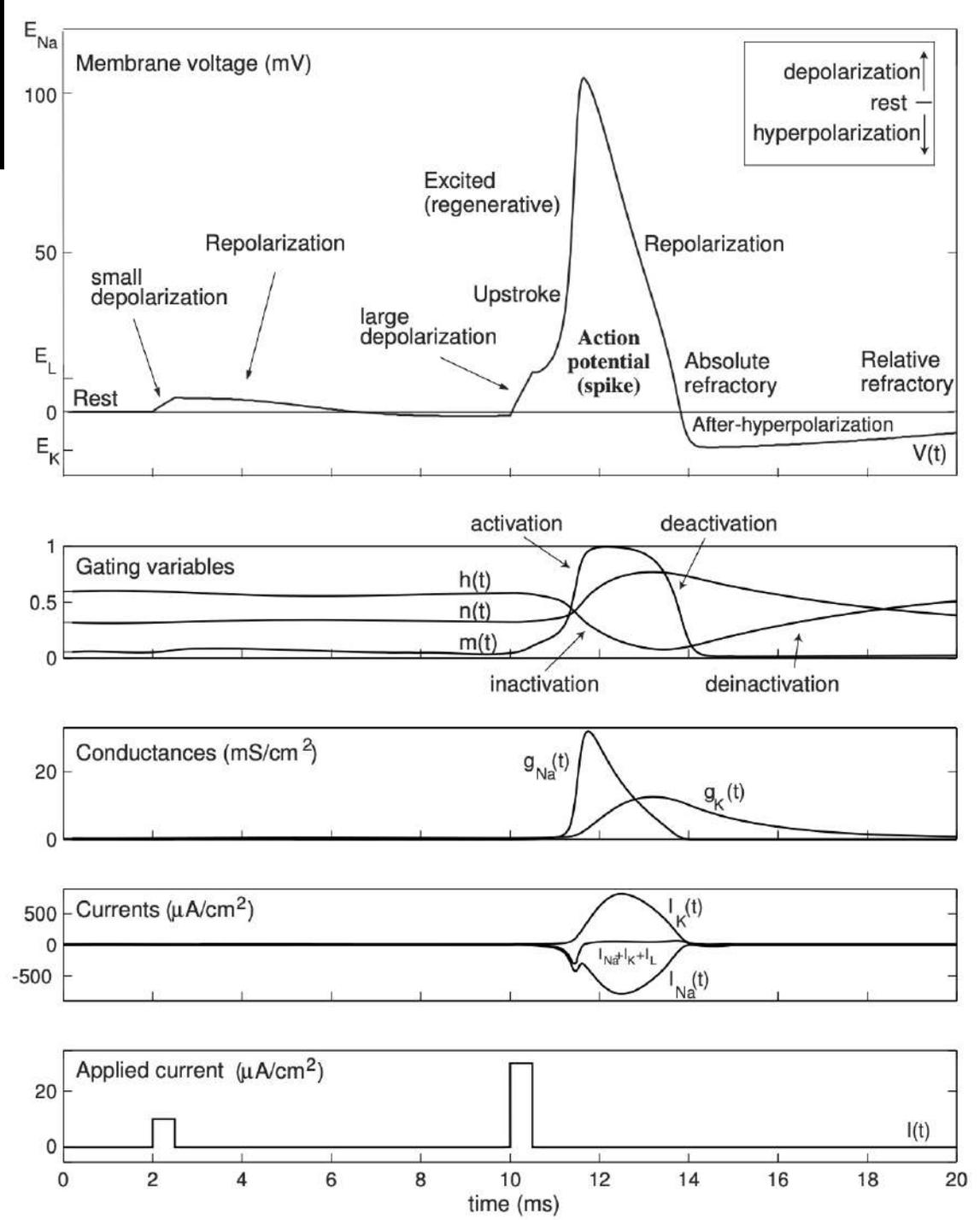
$$m_{\infty} = \alpha_m / (\alpha_m + \beta_m), \quad \tau_m = 1 / (\alpha_m + \beta_m),$$

$$h_{\infty} = \alpha_h / (\alpha_h + \beta_h), \quad \tau_h = 1 / (\alpha_h + \beta_h)$$





# The Hodgkin – Huxley model





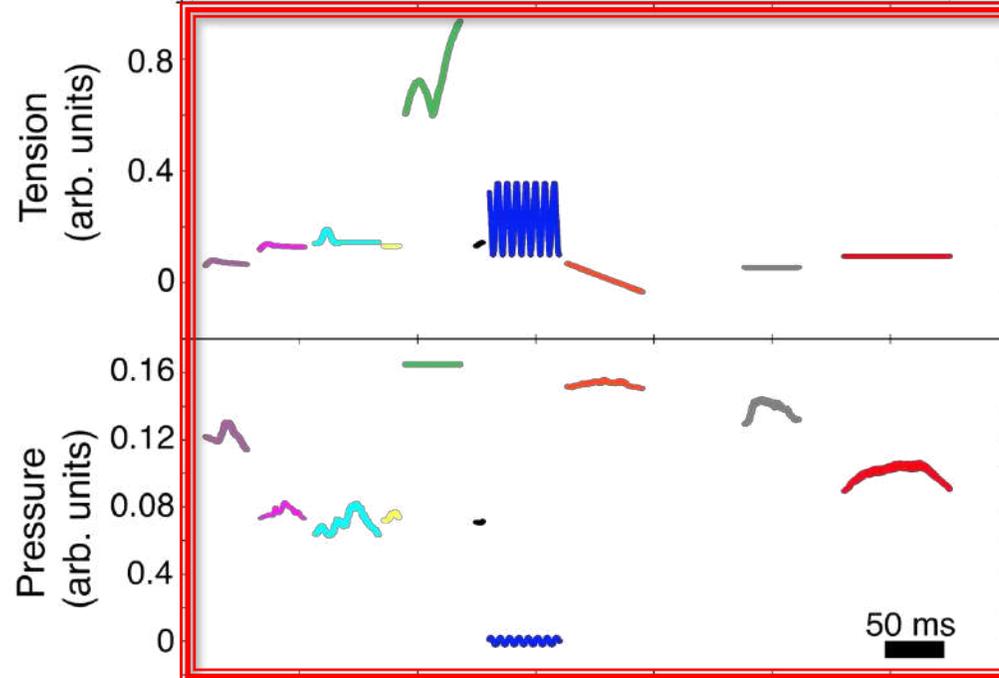
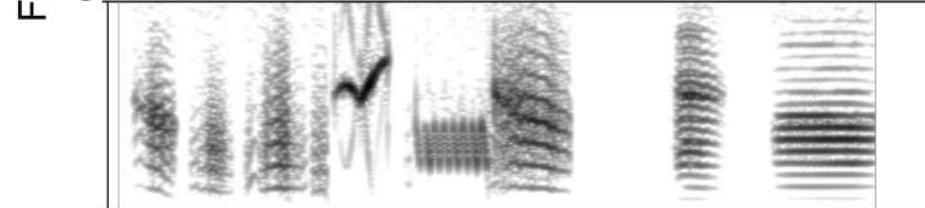
# Our approach to biomechanics



BOS



SYN



The birdsong model provides a code in terms of  $\alpha$  (pressure) and  $\beta$  (tension). We fit these parameters so that BOS and SYN have:

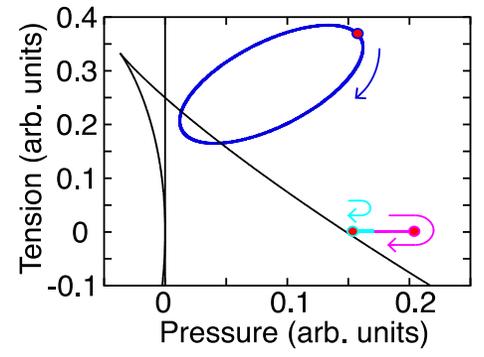
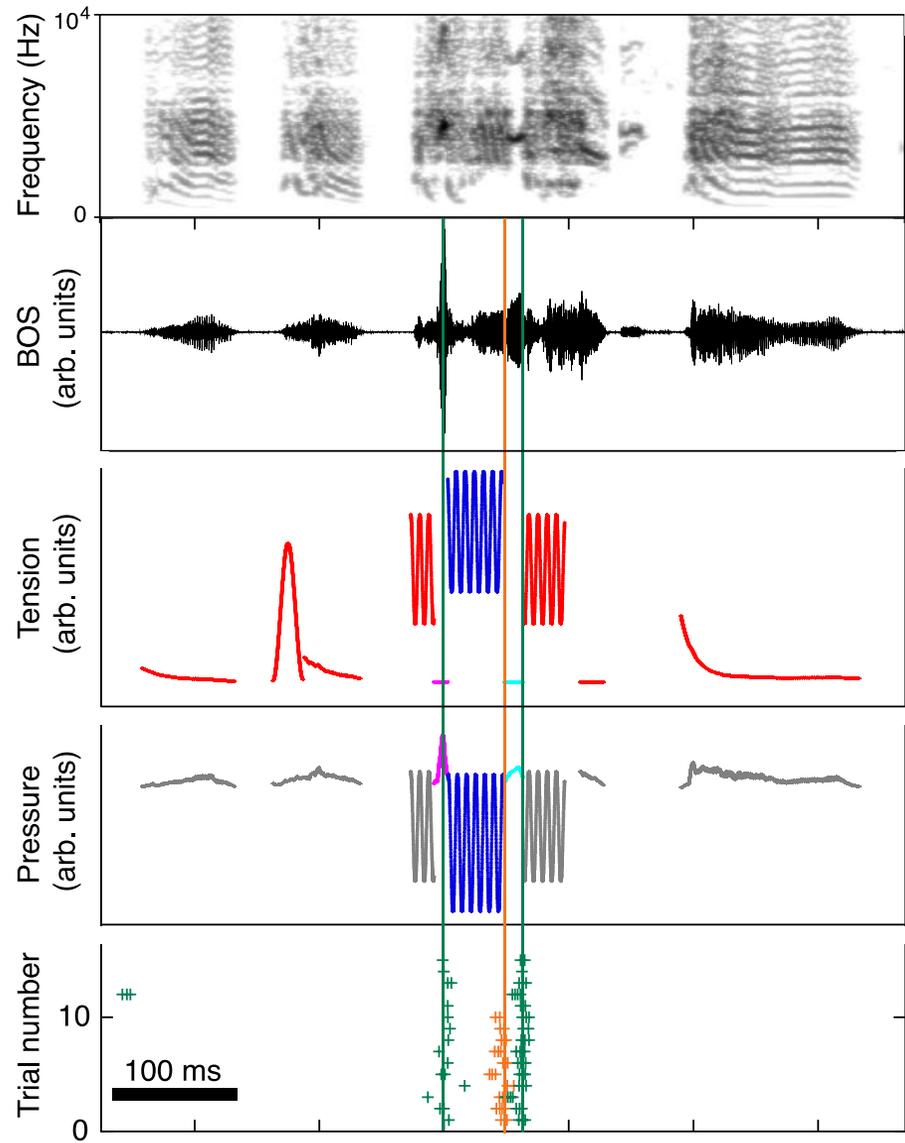
- ✓ Same fundamental frequency
- ✓ Same spectral content

Emergence of “motor gestures”

# Using the model to unveil the neural code



Sleeping birds

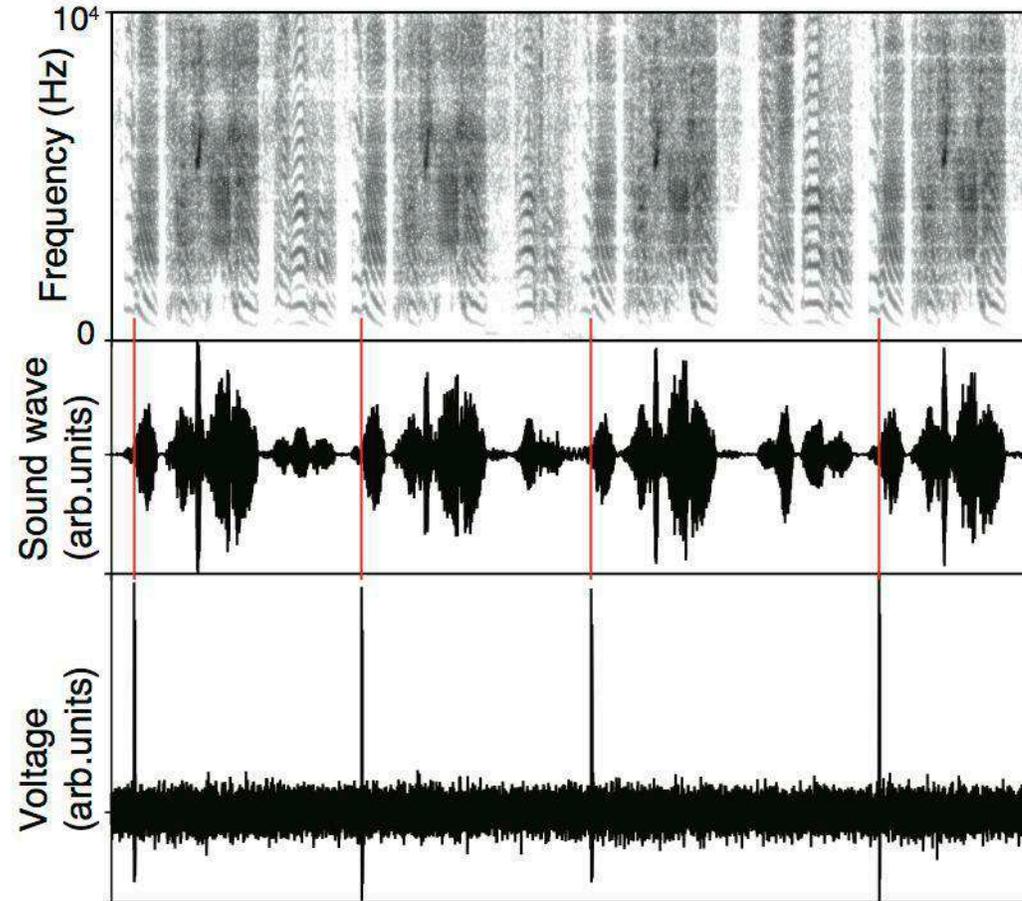


GTE Gesture  
Trajectory  
Extrema

# Using the model to unveil the neural code



Singing birds



Song

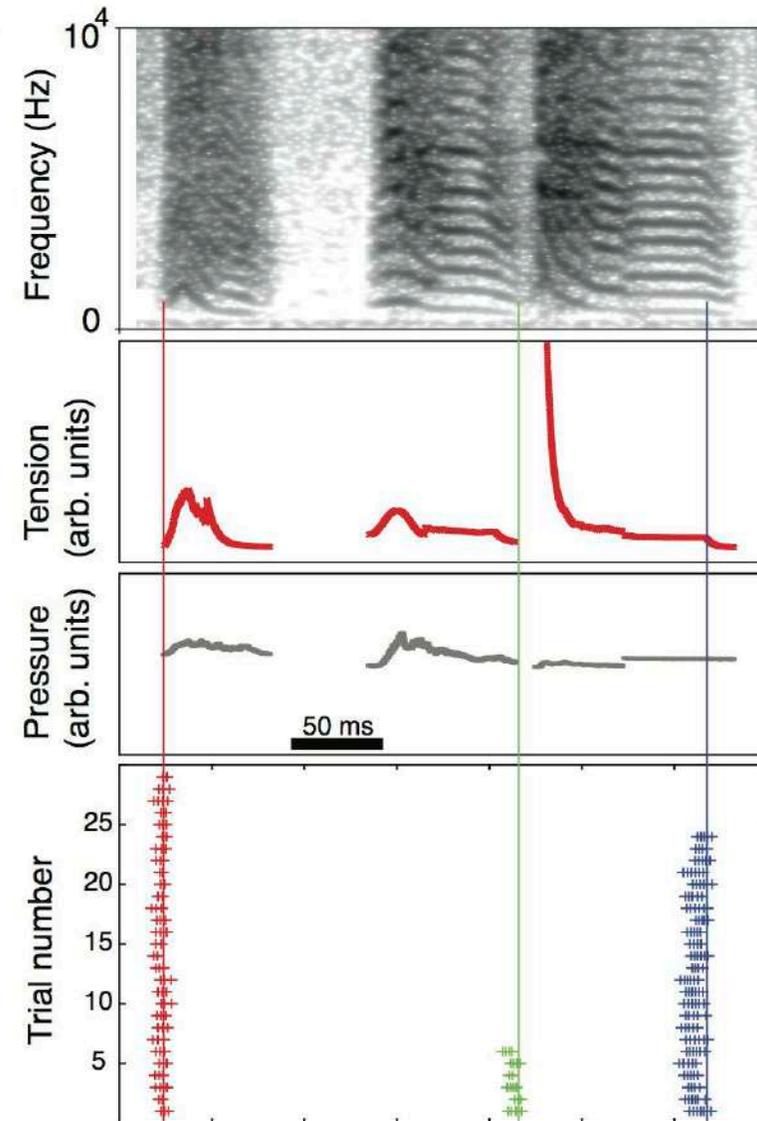
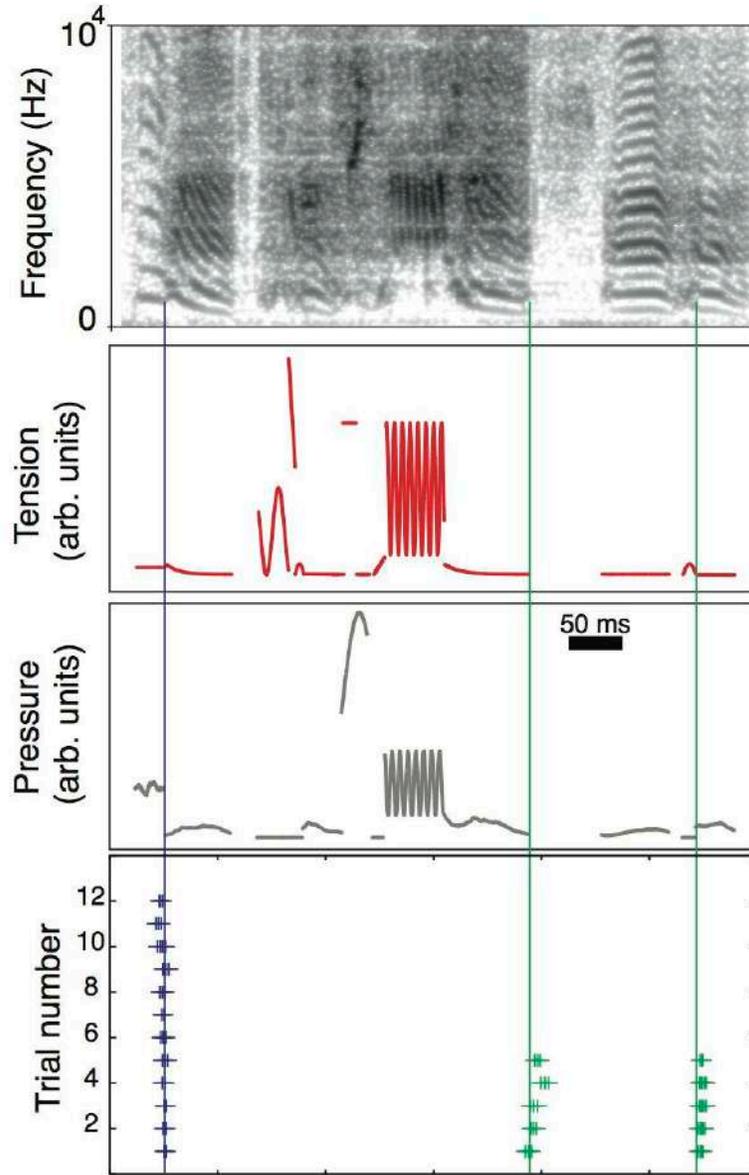
Neural activity

# Using the model to unveil the neural code



Singing  
birds

Neurons fire  
at significant  
motor  
instances





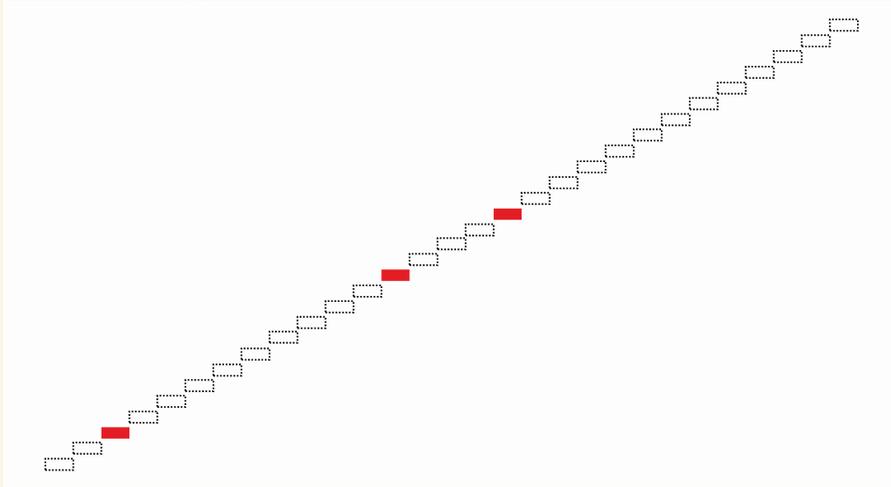
# Two hypothesis



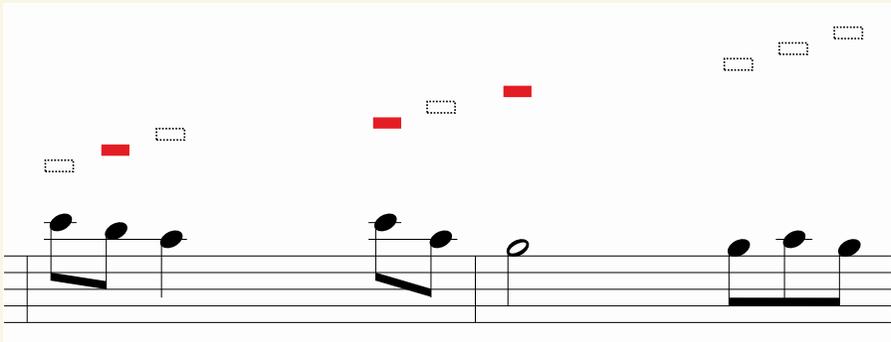
Recorded activity



a Clock hypothesis

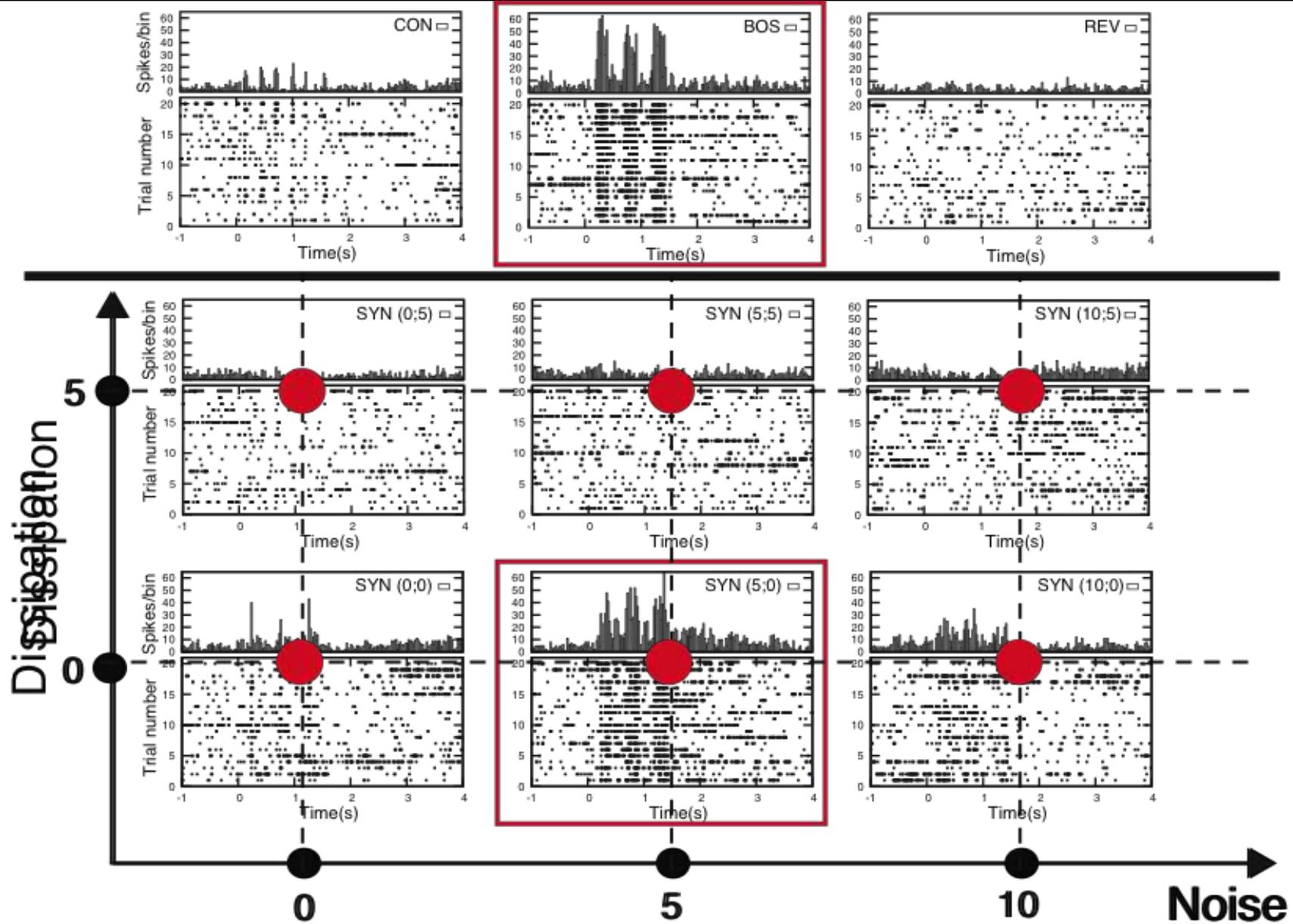


b Gesture-transition hypothesis



Modified from  
Troyer,  
Nature 2013

# Tonic neurons



# Also, in a singing bird



- Neurons code for significant motor instances.
- Predictive model

